Changes in myocardial echo amplitude during reversible ischaemia in humans

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Abstract

Objective—This study investigated the changes in regional myocardial ultrasonic backscatter, measured as myocardial echo amplitude, that occur during reversible myocardial ischaemia in humans.

Design—Left anterior descending coronary angioplasty was used to produce reversible myocardial ischaemia in human subjects. Regional myocardial echo amplitude was studied in the interventricular septum and left ventricular posterior free wall before, during, and after coronary occlusion with the angioplasty balloon. Wall motion analysis of the left ventricle was performed from simultaneous cross sectional echocardiographic imaging. Patients were studied prospectively.

Patients—Six patients (mean age 56 (SD 11), range 46 to 69 years) with single vessel left anterior descending coronary artery stenoses, were investigated during elective coronary angioplasty. A total of 11 balloon inflations were studied.

Setting—All patient studies were performed at Harefield Hospital. Echo amplitude analysis was performed at the Royal Brompton Hospital.

Interventions—Angioplasty was performed by the usual procedure at Harefield Hospital for elective coronary angioplasty. All routine medication including β blockers and calcium antagonists were continued. Inflation pressures were up to 12 atm (1212 kPa) and mean inflation time ranged from 30 to 120 (86 (31)) s. In four studies the first inflation was examined, in three the second, in two the third, and in one each the fourth and fifth inflations. Echo amplitude and cross sectional echocardiographic studies were recorded with a 3-5 MHz Advanced Technology Laboratories (ATL) (720A/8736 series) mechanical sector scanner and an ATL Mark III (860-1 series) echocardiograph system with 45 dB logarithmic grey scale compression.

Main outcome measures—Regional echo amplitude was examined in four regions of the left ventricle—namely, the basal and mid-septum, and basal and mid-posterior wall. Consecutive end diastolic and end systolic frames were analysed and cyclic variation was determined as the difference between the level of echo amplitude at end diastole and at end systole. Measurements were made before balloon inflation, at peak inflation, and after balloon deflation. Regional wall motion and systolic wall thickening were analysed qualitatively.

Results—Before balloon inflation, cyclic variation in echo amplitude was noted in all regions (basal septum, 2.4 (SD 1.1) dB; mid-septum, 2.5 (1.1) dB; basal posterior wall, 3.3 (2.1) dB; mid-posterior wall, 3.9 (1.6) dB). During balloon inflation there was a significant fall in cyclic variation to 0.4 (0.9) dB (p < 0.0002) in the mid-septum. This was predominantly owing to an increase in end systolic echo amplitude from 5.4 (2.0) dB to 9.3 (1.9) dB (p < 0.01). This was associated with the development of severe hypokinesis or akinisia in the mid-septum. No significant changes in echo amplitude occurred in the three other regions examined. Changes were completely reversed after balloon deflation.

Conclusions—These results suggest a causal relation between occlusion of the supplying coronary artery and blunting of myocardial echo amplitude cyclic variation. It is suggested that balloon occlusion produced myocardial ischaemia. The resultant impairment of myocardial contraction then caused a blunting of cyclic variation in echo amplitude. The results of this study provide further data about the ability of quantitative studies of ultrasonic backscatter to identify alterations in the myocardium during injury.

A link between cyclic variation in echo amplitude and cardiac contraction has been shown. To assess this relation further a human model of reversible myocardial ischaemia was used to examine the effect of a reversible perturbation of cardiac contraction on cyclic variation of echo amplitude. Percutaneous transluminal coronary angioplasty of the left anterior descending artery provided an ideal model for studying left ventricular performance and function during short, controlled, and reversible episodes of myocardial ischaemia. Catheter balloon inflation performed during coronary angioplasty produces virtually total interruption of regional coronary blood flow. Numerous studies during coronary angioplasty have
shown the effect of balloon occlusion on global and regional left ventricular function using either M mode or cross sectional echocardiography, direct cine left ventriculography, and intravenous digital subtraction ventriculography. Similarly left ventricular filling dynamics have been studied during coronary angioplasty with high fidelity manometer tipped catheters and Doppler echocardiography. These studies suggested that coronary angioplasty provided an ideal model in which to study the effect of reversible myocardial ischaemia on cyclic variation in echo amplitude. As left anterior descending coronary artery angioplasty had been shown to produce changes in segmental shortening in the distal and mid-intraventricular septum, cyclic variation in echo amplitude was examined in this region of the myocardium in a series of patients with single vessel left anterior descending stenoses who were undergoing coronary angioplasty.

Patients and methods

PATIENTS

Six patients with single vessel left anterior descending coronary artery disease, defined as greater than 70% luminal stenosis, were investigated during elective coronary angioplasty. No patient had a history of transmural myocardial infarction. Two patients were women and patient age ranged from 46 to 69 years (mean (SD) 56 (11) years). All patients previously had diagnostic coronary angiography and cine left ventriculography in the 30° right anterior oblique projection performed for the investigation of angina. In all cases left ventriculography was normal or showed minimal anterior hypokinesia only. A total of 11 balloon inflations were studied in the six patients; three inflations in one, two inflations in three, and one inflation each in the remaining two. The study was approved by the hospital ethical committee and all patients gave informed consent. Care was taken not to interfere with or prolong the therapeutic procedure. Table 1 shows characteristics of the patients.

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Table 1 Coronary angioplasty patient characteristics

PERCUTANEOUS TRANSLUMINAL CORONARY ANGIOPLASTY PROTOCOL

Angioplasty was performed by the usual procedure for elective coronary angioplasty at Harefield Hospital. Patients were premedicated with intramuscular papaveretum and metoprolamide. All routine medication including β blockers and calcium antagonists was continued.

The angioplasty procedure was performed via the femoral approach. An intravenous single dose of 5000 units of heparin was administered at the start of the procedure. Non-ionic contrast medium, steerable guide wires, and balloon catheters with diameters varying from 2.5 to 3.5 mm were used. Inflation pressures were up to 12 atmospheres (1212 kPa) and mean inflation time (86 (SD 31)) ranged from 30 to 120 s. Table 2 shows that in four studies the first inflation was examined, in three the second, in two the third, and in one each the fourth and fifth inflations.

Continuous electrocardiographic monitoring was performed throughout the procedure with the six limb and augmented limb leads (I, II, III, aVL, aVF, and aVR) being monitored by a 7 series Siemens Elema Mingograf. The electrocardiogram was recorded immediately before and throughout each balloon inflation and after balloon deflation until any changes had resolved.

ECHO AMPLITUDE AND CROSS SECTIONAL ECHOCARDIOGRAPHY STUDIES

Echo amplitude and cross sectional echocardiographic studies were recorded with a 3.5 MHz Advanced Technology Laboratories (ATL) (720A/8736 series) mechanical sector scanner and an ATL Mark III (860–1 series) echocardiograph system with 45 dB logarithmic grey scale compression. To obtain the least modified echo amplitude signal, self correcting circuits were inactivated to avoid further differentiation of the original echo signal. Images were simultaneously displayed in grey scale and in colour by a Brompton Encoder (Alltek Hospital Supplies, Shepperton, Middlesex, UK) as they were recorded. On the colour scale each level of echo amplitude was represented as a single colour in the sequence: cyan, green, yellow, red, magenta, blue, and white, the last corresponding to maximum amplitude. The brightness of the displayed signal was modulated so that within each colour level, the luminosity was varied. This approach allowed a continuous range of echo amplitude to be displayed, and also meant that regions of low echo amplitude appeared with low brightness on the screen. These were less conspicuous on the final image and thus preserved the original amplitude perspective.

All images were acquired with a standardised protocol to enable intrapatient and interpatient comparisons. Patients were studied in the supine position and long axis parasternal views were recorded. Gain settings were standard-
ised: the master gain was increased until the parietal pericardium posterior to the left ventricle was just displayed at the highest level of the encoder (white). The depth compensation was then set to a linear ramp across the image at a rate of roughly 2 dB/cm. The gain settings were not altered thereafter. Images were stored on U-matic 3/4 inch video tape in a Sony VO 5800PS recorder.

Image analysis was performed by a Tandem PDA desk top computer. Stop frame end diastolic and end systolic images for analysis were selected by a video recorder with digital frame advance (Sony VO 5800PS). These frames were transferred from tape to a 512 × 256 × 6 bit frame store. Images were processed with an adaptive filtering process for the reduction of speckle as this decreased echo amplitude variance and allowed smaller sample sizes to be used.12 Four areas of interest were defined, in the interventricular septum (basal and mid-septum), and posterior wall (basal and mid-posterior wall) as defined by the American Society of Echocardiography (ASE).13 Measurements of 256 individual picture elements (pixels) were made from each area. Four separate measurements, each of 64 pixels, were made and averaged rather than one individual measurement of 256 pixels as this allowed the pixel matrix to be placed within the mid-myocardium and thus avoided including specular echoes from the endocardium or epicardium. A maximum pixel intensity for each image was derived by measuring the maximum colour intensity of the superimposed colour scale (usually corresponding to 52 levels of grey scale). This corresponded to a value of 45 dB and allowed echo amplitude values (dB) to be assigned (a grey scale level thus corresponding to approximately 0-86 dB). Individual pixel amplitudes were displayed as a histogram and a separate digital readout displayed mean, median, and SD values for each region measured. The display of the frequency histogram on the image proved useful, as an obviously bimodal form usually meant that specular echoes had mistakenly been included in the area of interest. Consecutive end diastolic and end systolic frames were analysed and cyclic variation determined as the difference between the level of echo amplitude at end diastole and at end systole. Cyclic variation index was calculated as the ratio: cyclic variation (end diastolic echo amplitude minus end systolic echo amplitude): end diastolic echo amplitude.

Images for analysis were recorded at baseline with the deflated balloon and guide wire across the coronary lesion, at the peak of balloon inflation and after balloon deflation. In order not to interfere with the therapeutic procedure and patient safety and welfare, the timing of the imaging after deflation was by necessity variable. Seven balloon inflation images were acquired 15-30 seconds after deflation, but in the remaining four inflations, images could not be acquired until five, 10, 20, and 60 minutes after balloon deflation. In one study images of the mid-posterior wall were not suitable for analysis.

Regional wall motion analysis was performed qualitatively. Normal left ventricular wall motion was assessed by the amount of systolic myocardial thickening and inward endocardial motion. Abnormalities of segmental wall function were identified by a reduction in wall thickening and motion.

### Results

#### Clinical Outcome, Chest Pain, and ST Segment Changes

All six patients underwent successful dilatation of their coronary stenoses. Significant ST segment shifts on the monitored electrocardiographic leads occurred during five balloon inflations. This was accompanied by chest pain consistent with cardiac ischaemia during three inflations (table 2). On all occasions ST segment changes and chest pain resolved rapidly after balloon deflation.

#### Wall Motion and Thickening Abnormalities

Before balloon inflation no significant wall motion abnormalities were present. During each of the 11 balloon inflations, severe hypokinesis or akinesia developed in the mid-septum and distal septum accompanied by diminished or absent wall thickening. Obvious hyperkinesis or severe hypokinesis of the ventricular wall was not seen elsewhere in the myocardium during any balloon inflation, except in the distal mid-posterior wall of two patients (patients 1 and 2). In the seven inflations where imaging was obtained for the first 30 seconds after balloon deflation the hypokinesis or akinesia seen resolved within the 30 s after deflation. For the remaining four inflations, resolution of the wall motion abnormalities was noted at the time of imaging after deflation.

### End Diastolic and End Systolic Regional Echo Amplitude

Table 3 shows mean values for regional echo amplitude for all four regions of ventricular myocardium at both end diastole and end systole. Tables 4-7 show the individual values for all patients. Values were greatest at end

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<th>Table 3 Mean end diastolic and end systolic echo amplitude values during percutaneous transluminary coronary angioplasty (mean (SD))</th>
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<td>ES (dB)</td>
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<tr>
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<td>ED (dB)</td>
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<td>ES (dB)</td>
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<td>ED (dB)</td>
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<td>ES (dB)</td>
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*p < 0.0001 (ANOVA) for all four groups, p < 0.05 for all patients (Bonferroni) comparing the mid-septum to other regions. Basal PW, basal posterior wall; ED, end diastole; ES, end systole; Mid-PW, mid-posterior wall.
Table 4 Individual echo amplitude (dB) at the basal septum for end diastole (ED) and end systole (ES) during angioplasty

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CVI, cyclic variation index.

diastole, and least at end systole. There was no significant difference between pre-inflation or post-inflation values at end diastole or end systole for the four regions. End systolic values in the mid-septum at peak inflation, however, were significantly greater (p < 0.005) than values for the other three regions of myocardium examined. For the mid-septal region, systolic values of echo amplitude were greatly increased by peak inflation compared with pre-inflation (p < 0.01) After balloon deflation, values fell significantly (p < 0.01) and returned to values not significantly different from pre-inflation values.

Cyclic Variation in Echo Amplitude

Table 8 shows mean values for cyclic variation. Tables 4-7 shows individual values for cyclic variation index. Values for pre-inflation and post-inflation were not significantly different for the four regions for either the absolute value of cyclic variation of echo amplitude (end diastolic echo amplitude minus end systolic echo amplitude) or the cyclic variation index. At peak inflation there was a significant fall in both these variables in the region of the mid-septum (ANOVA, p < 0.001) compared with both pre-inflation (Bonferroni’s (comparison of pairs), p < 0.002 and p ≤ 0.01 respectively) and post inflation (Bonferroni’s, p < 0.0002 and p ≤ 0.01) values. This major decrease in cyclic variation was not seen in the other three regions of myocardium examined (figure).

Summary of Results

During balloon inflation the mid-septum and distal septum of the ventricle became severely hypokinetic or akinetic. These changes were accompanied by significant changes in echo amplitude in the mid-septum. In this region a noticeable increase in end systolic echo amplitude occurred resulting in a fall in cyclic variation in echo amplitude to 16% of pre-inflation values and a similar fall in cyclic variation index to 10% of pre-inflation values. These changes paralleled the decrease in wall thickening seen qualitatively. After balloon deflation these changes reverted to pre-inflation values as did wall thickening.

Table 5 Individual echo amplitude (dB) at the mid-septum for end diastole (ED) and end systole (ES) during angioplasty

<table>
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<tr>
<th>Patient</th>
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CVI, cyclic variation index.

Discussion

This study documents the effects of reversible coronary artery occlusion on cyclic variation of myocardial echo amplitude. In the mid-septal region of the left ventricular myocardium, after balloon occlusion of the supplying left anterior descending coronary artery, regional cyclic variation in echo amplitude was much blunted, falling to values less than 16% of pre-occlusion values. Cyclic variation index, which relates the level of cyclic variation to end diastolic levels of echo amplitude, also declined significantly to less than 10% of pre-occlusion values. These changes were completely reversible after balloon deflation suggesting a causal relation between occlusion of the supplying vessel and the blunting of cyclic variation. It is postulated that balloon coronary artery occlusion produced myocardial ischaemia in the territory of the left anterior descending coronary artery. The resultant impairment of myocardial contraction subsequently caused a blunting of cardiac cycle dependent variation in back-scattered ultrasound. After balloon deflation and reperfusion these changes were rapidly reversed with no permanent sequelae. The evidence for this postulate is discussed further.
Table 6 Individual echo amplitude (dB) at the basal posterior wall for end diastole (ED) and end systole (ES) during angioplasty

<table>
<thead>
<tr>
<th>Patient</th>
<th>Variable</th>
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<th>Peak inflation</th>
<th>Post-infusion</th>
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CVI, cyclic variation index.

**EVIDENCE FOR MYOCARDIAL ISCHAEMIA**

**Clinical findings**

An early manifestation of acute myocardial ischaemia is the development of ST segment change on the electrocardiogram. Such changes were noted during five of the 11 balloon occlusions in this study. Previous studies in which limb lead electrocardiograms only were monitored have shown similar findings. Hauser et al found ST segment shift in seven of 16 patients undergoing left anterior descending coronary angioplasty. Visser et al found ST segment change in four of 15 patients undergoing coronary angioplasty (10 single vessel left anterior descending, four single vessel right coronary artery, and one double vessel right coronary artery and left anterior descending coronary artery). The use of 12 lead electrocardiographic monitoring greatly increases the frequency of ST segment change noted. In a group of 32 patients with mixed single and multiple vessel disease of whom 17 had angioplasty of the left anterior descending coronary artery, Labovitz et al analysed electrocardiograms to find significant ST segment changes in 25 of 31. Wohlgelernter et al detected ST segment changes in 12 of 14 patients during angioplasty of the left anterior descending coronary artery and Norell et al in 33 of 52 patients. The use of intracoronary electrograms, recorded via the tip of the angioplasty guide wire positioned distal to the coronary stenosis being treated, greatly increased the yield of ST segment changes.

In a study by Jain and Gettes ST segment change occurred in 33 of 35 patients undergoing left anterior descending coronary angioplasty but was simultaneously detected in only 13 patients by observation of surface leads II and V1. The absence of ST segment change in over half (six of 11) of the balloon occlusions examined in our study does not therefore exclude acute myocardial ischaemia during those occlusions. Similarly the occurrence of chest pain during only three of 11 balloon inflations was consistent with that previously reported. Hauser et al reported chest pain in eight of 16 patients during left anterior descending coronary angioplasty, and Visser et al in five of 15 patients although only 11 of these patients underwent left anterior descending coronary angioplasty, the remainder being right coronary artery lesions. The absence of chest pain would appear to correlate poorly with the absence of acute myocardial ischaemia, chest pain being the last manifestation of ischaemia.

**Wall motion and systolic wall thickening**

Coronary artery ligation in open chested dogs causes echocardiographically detectable systolic wall thinning in the ischaemic region within 30 s. In our study, decreased systolic wall thickening was noted in the distal and mid-interventricular septum during all 11 balloon inflations studied. Similar findings have been well documented by other workers. Hauser et al found new or increased wall motion abnormalities in 14 of 16 patients during left anterior descending coronary angioplasty. Hypokinesia was noted within 33 (19 (70)) s of balloon occlusion in all 14 patients and invariably preceded ST segment shift or chest pain where these occurred. Wall motion returned to normal within 30 seconds of balloon deflation in 12 of these patients. Alam et al studied eight patients with left anterior descending single vessel coronary artery disease during 14 balloon occlusions and noted a fall in systolic wall thickening of 50% or more in the interventricular septum during 13 of these occlusions.

(Table 7 Individual echo amplitude (dB) at the mid-posterior wall for end diastole (ED) and end systole (ES) during angioplasty)

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*Not analysable; CVI, cyclic variation index.*
Wall thickening abnormalities began within 20 s of balloon inflation in all 13 cases and returned to pre-occlusion levels within 20 s of balloon deflation. Visser et al documented similar wall motion abnormalities developing in 15 patients during 49 balloon inflations at a mean of 8 (3) s after balloon inflation. A wall motion returned to baseline in all patients 19 (8) s after balloon deflation. Again Wohlgelernter et al reported 14 patients each undergoing angioplasty of an isolated left anterior descending stenosis who all developed severe hypokinesia (29%) or akinesia (71%) of the septal and apical region of the left ventricle by balloon inflation lasting 60 s. Recovery to pre-occlusion values began within 15 (5) s (range 6 to 22) and was complete in all patients by 70 s after inflation with a mean time to full recovery of 43 (17) s. Evidence that ischaemia is the cause of the wall motion abnormalities recorded echocardiographically was provided by techniques to improve myocardial perfusion distal to the occluding angioplasty balloon. Timmis et al infused arterial blood through the angioplasty catheter into the distal coronary artery in 10 patients during 60 s balloon occlusions. These inflations were compared with control occlusions with either no distal infusion or distal infusion with Hartman's solution. All dilatations without blood infusion in the 10 patients produced regional wall motion abnormalities within 16-0 (3-2) s. By contrast only one dilatation with distal blood infusion produced wall motion abnormalities. Infusion with Hartman's was not helpful in limiting wall motion abnormalities suggesting that oxygen delivery via arterial blood, rather than wash out of metabolites, was responsible for the benefit. Jaffe et al studied 42 patients undergoing coronary angioplasty using distal transcatheter coronary perfusion with oxygenated Fluosol DA (20% emulsion), a perfluorocarbon oxygen transport fluid. They found a dramatic fall in left ventricular regional wall motion abnormality during perfusion with oxygenated Fluosol DA compared with controls. It seems that the development of regional wall motion abnormalities during coronary angioplasty not only reflects myocardial ischaemia but is also a sensitive and early marker of it. The development of regional wall motion abnormalities during coronary angioplasty in this study seem to reflect underlying myocardial ischaemia in the territory supplied by the left anterior descending coronary artery.

**Cyclic Variation in Regional Backscattered Ultrasound**

In 1983 and 1984, Madaras et al and Barzilai et al first reported cyclic variation in backscattered myocardial ultrasound. They analysed myocardial integrated backscatter as a measure of backscattered ultrasound and examined this in a dog model after occlusion of the left anterior descending artery. Cyclic variation in integrated backscatter was significantly blunted in ischaemic areas of myocardium. These areas were previously delineated at open thoracotomy during brief coronary occlusion. The effects of reperfusion were not studied in this model. In a later study using a similar open chest dog model, cyclic variation in integrated backscatter was examined during coronary occlusion and after two hours of reperfusion. Cyclic variation at the left ventricular apex in the four dogs studied was 5-6 (1-4) dB at baseline and fell to 0-4 (1-5) dB after 10 min of occlusion (p < 0-02). After two hours of reperfusion, values were not significantly different from baseline at 3-9 (1-2) dB. Cross sectional echocardiographic apical four chamber views of the apex showed dyskinesis and loss of systolic thickening after 10 min of occlusion. This was substantially but not completely restored to baseline values after two hours of reperfusion. Corresponding values for systolic wall thickening at the apex were: baseline, 63-4 (17-7)%; 10 min occlusion, 2-2 (11-5)% (p < 0-001); two hours reperfusion, 52-9 (26-8)% (NS). Similar effects of ischaemia on cyclic variation of backscattered ultrasound from dog myocardium after coronary artery occlusion have been found by several other workers. Cyclic variation in backscattered myocardial ultrasound has also been found in humans.

---

**Table 8**  
Mean (SD) cyclic variation in echo amplitude and cyclic variation index during angioplasty

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<th></th>
<th>Pre-inflation</th>
<th>Peak inflation</th>
<th>Post inflation</th>
<th>p Value for all paired groups (Bonferroni)</th>
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<td>(dB)</td>
<td>(dB)</td>
<td>(dB)</td>
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<td>Cyclic variation in echo amplitude</td>
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<td></td>
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<td>2-4 (1-1)</td>
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</table>

* p < 0-0001 (ANOVA) for all four groups, comparing the mid-septum with other regions. Basal PW, basal posterior wall; Mid-PW, mid-posterior wall.
This has been shown by integrated backscatter,26–29 grey scale echo amplitude,30 and colour encoded echo amplitude.1 The effect of ischaemia on cyclic variation in backscattered ultrasound in humans is limited. Milunski et al studied 21 patients in a cardiac care unit within the first 24 hours after the onset of symptoms suggestive of acute myocardial infarction.28 Areas of ischaemic injury were identified by cross sectional echocardiography and electrocardiography. Cyclic variation of integrated backscatter was measured in these areas and normal control areas of myocardium. The coronary artery bypass was given to 17 patients. Cyclic variation in normal regions was 4-8 (0-5) dB compared with 0-8 (0-3) dB (p < 0-05) in regions with infarction. In the 15 patients who were serially studied and also underwent coronary angiography to define vessel patency, 10 had patent infarct related coronary arteries. In these patients the magnitude of cyclic variation increased with time (1-3 (0-6) dB to 2-5 (0-5) dB, p < 0-05) where in those with occluded infarct related vessels no significant recovery was seen (0-3 (0-3) dB to 0-6 (0-3) dB, NS). It was concluded that the reduction of cyclic variation in the patent vessel group represented the beneficial effect of reperfusion. Significantly the improvement in cyclic variation shown in this group was not accompanied by a noticeable improvement in wall motion.

It is probably incorrect, however, to compare the brief periods of coronary occlusion during clinical angioplasty with the prolonged periods of coronary occlusion in the study of Milunski et al,28 and the animal studies already mentioned in which coronary occlusion times greater than five min were used. Many investigators have shown that although partial recovery of myocardial contractile function after brief ischaemia occurs promptly, complete recovery may require longer periods of reperfusion.32–35 With more prolonged periods of myocardial ischaemia (>5 min) it is likely that structural changes are occurring. Myofibril stretching after similar periods of ischaemia are well described34 as are other ultrastructural changes.35 Zhao et al found disruption of the collagen matrix of dog myocardium with accompanying persistent myocardial dysfunction, after 12 sequential five min occlusions of the left anterior descending coronary artery.35 This was unaccompanied by irreversible cellular damage. Therefore it is not surprising that cyclic variation may not be fully restored after several hours of reperfusion if ischaemia is prolonged more than a few minutes with resultant damage to cellular and extracellular structures. This contrasts with the rapid recovery of both myocardial systolic function and cyclic variation in echo amplitude that occurred with coronary reperfusion, after balloon deflation during angioplasty, which this study documents.

One other study, by Hajduczki et al37 has documented changes in backscattered ultrasound during coronary angioplasty in humans. They examined patients during left anterior descending coronary angioplasty and showed a substantial change in cyclic variation of backscatter during balloon inflation. Backscatter fell from 8-6 (3-3) units pre-inflation to 3-2 (1-7) units at peak inflation (p < 0.001). They did not comment on whether this reversed after balloon deflation. They also noted an increase in cyclic variation of backscatter in areas of myocardium that were identified as hyperkinetic during balloon inflation. In our study the grouped data did not show a significant increase in cyclic variation of backscattered ultrasound in either basal segments of the left ventricle (where hyperkinesis would be most likely to occur) during balloon inflation, although increases in cyclic variation index of >10% were noted in both areas during two of the 11 inflations (tables 4, 6).

There are several explanations for the changes in cyclic variation that occur in association with myocardial ischaemia. Wickline et al have suggested a mechanism to explain cyclic variation in backscattered myocardial ultrasound (in their case integrated backscatter).38 They suggested a relation between cyclic variation in integrated backscatter and myocardial contractile function which reflects cyclic variations in myofibrillar elastic parameters, with the juxtaposition of intracellular and extracellular elastic elements that have different intrinsic acoustic impedances providing an appropriately sized scattering interface at the cellular level. Because acoustic impedance mismatch is partially determined by elastic modulus, changes in local elastic moduli which result from myocardial elastic elements not obeying Hook’s law as they are stretched, may alter the degree of impedance mismatch. With a simple Maxwell type muscle model to depict cardiac cell mechanical behaviour, a model employing an extracellular parallel elastic element and intracellular series elastic and contractile elements can be constructed. This model predicts the decrease in backscattered ultrasound found during systole. Cardiac cycle dependent alterations in the degree of local acoustic impedance mismatch may therefore elicit concomitant changes in backscattered ultrasound. More recently Rijsterborgh et al confirmed in animal studies that the higher systolic backscatter seen during ischaemia could be explained by the decrease in wall thickness that occurs with ischaemia and not by the ischaemia itself, in keeping with the influence of myocardial contraction on cyclic variation.39 Other possibilities include alterations in the relative insonifying angle due to changing fibre angle and shape during the cardiac cycle as it is known that both reflection and attenuation of ultrasound alter according to the direction of fibre insonification.40 Whatever the exact basis of cyclic variation in backscattered ultrasound, there is no doubt an important relation with contractile events occurring within the myocardium at either a cellular or fibre level. As myocardial ischaemia occurs these contractile events are disrupted and cyclic variation as a result is blunted. Changes in myocardial blood flow during coronary occlusion must also be considered as a cause of the blunting of cyclic variation in
backscattered ultrasound, as changes in red blood cell concentration have been shown to noticeably affect overall levels (as distinct from cyclic variation) of backscattered ultrasound in experimental models.\(^\text{3,4-13}\) Wickline et al, however, in a series of experiments on perfused and non-perfused dog hearts that were cyclically distended and relaxed by an intracavitary ventricular balloon, showed that myocardial perfusion with whole blood did not contribute significantly to the phenomenon of cyclic variation in backscattered ultrasound.\(^\text{14}\)

Importantly, in this study there was an increase in end diastolic echo amplitude in the mid-septum during balloon inflation from 8-4 (2-2) dB to 9-7 (2-1) dB that is significant (p < 0-05) if the mid-septum alone is considered. This would be consistent in a fall with in concentration of formed blood elements in the myocardium during coronary occlusion.\(^\text{15}\)

### Conclusion

It is likely that balloon coronary occlusion during angioplasty results in reversible myocardial ischaemia which produces a reversible blunting of cardiac cycle dependent backscattered ultrasound after temporary contractile dysfunction induced by ischaemia. The results of this study are consistent with this hypothesis and provide further data on the ability of techniques involved in the quantitative study of backscattered ultrasound to clarify alterations in the myocardium during injury.

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PLANTS IN CARDIOLOGY

Fagarine

In 1932 G Stuckert was the first to isolate a new alkaloid, fagarine, from the Argentinian plant *Fagara coco* (Rutaceae); and with A Sartori he showed that it had a depressant action on the myocardium of rabbits. Further work at the University of Cordoba by Moisset de Espanes and others showed that fagarine raised the threshold for atrial and ventricular fibrillation in response to faradic stimulation, and that it decreased the incidence of ventricular fibrillation after coronary ligation in dogs. In all these experiments it was more effective than quinidine. Then A Taquini tried its effect in six patients with atrial flutter or fibrillation who were resistant to quinidine. In all of them intramuscular fagarine restored sinus rhythm within 30 minutes (*Science* 1945;102:69–70). In 1948 David Scherf showed that fagarine reliably reverted atrial fibrillation induced by aconitine in dogs (*Proceedings of the Society for Experimental Biology and Medicine* 1948;67:59–60).

The genus *Fagara* has been merged with *Zanthoxylum* and the name of the original *F coco* (Gill.) Engl. is now *Z coco* Gill ex Hook and Arn. The illustration is of a closely related species. The South African plant *Z capensis*, a “fever tree”, is used medicinally.

The family Rutaceae is widespread, especially in the tropics, and it includes *Pilocarpus microphyllus*, the source of pilocarpine. Citrus fruits belong to this family. Rutaceae is the fourth family of plants described in *Plants in Cardiology* with antiarrhythmic properties—quinidine, procaine, and lignocaine all being derived from other families. It would be interesting to know whether fagarine is still under investigation.

A HOLLMAN

Zanthoxylum fagara
Changes in myocardial echo amplitude during reversible ischaemia in humans.

D A Lythall, D G Gibson, S S Kushwaha, M S Norell, A G Mitchell and C J Ilsley

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