Assessment of infarcted myocardium with real time myocardial contrast echocardiography: comparison with technetium-99m sestamibi single photon emission computed tomography

P Tousek, M Orban, S Martinoff, C Firschke

Background: Little is known about the relation between the extent of microvascular damage and infarct size in patients after successful mechanical reperfusion of acute myocardial infarction.

Objective: To compare the spatial extent of reduced myocardial signal between real time myocardial contrast echocardiography (MCE) and single photon emission computed tomography (SPECT) after successful mechanical reperfusion of acute myocardial infarction and to test the hypothesis that MCE can be used for clinical infarct size assessment.

Methods: 10 days after successful mechanical reperfusion of acute myocardial infarction, 117 patients underwent MCE (power pulse inversion technique, slow contrast bolus injection) and SPECT (technetium-99m sestamibi). Location and number of segments with normal myocardial signal intensity and with mild and severe reduction were registered and the concordance between the techniques was calculated.

Results: Segmental concordance between MCE and SPECT was 83% (κ = 0.64). On average, the difference in the number of segments with reduced myocardial signal intensity between MCE and SPECT did not exceed one segment (p < 0.001). Sensitivity and specificity of MCE for the detection of an abnormal segment on SPECT were 87% and 91%, respectively. Intraobserver and interobserver agreement were 94% (κ = 0.84) and 92% (κ = 0.83), respectively.

Conclusions: Real time MCE is a promising technique for infarct size assessment after successful mechanical reperfusion of acute myocardial infarction.

The presence of myocardial microvascular damage despite successful reperfusion of acute myocardial infarction, myocardial “no reflow”, can be imaged with myocardial contrast echocardiography (MCE) and has been shown to be an indicator of unfavourable clinical prognosis.1 2 Little is known, however, about the relation between the extent of myocardial microvascular and myocellular damage—that is, infarct size, one of the key characteristics of patients with myocardial infarction.3 4 Whereas excellent agreement was obtained in the experimental setting,5 the results of previous clinical studies comparing intravenous MCE with single photon emission computed tomography (SPECT), the current reference standard of infarct size determination, were equivocal with some showing good and others poor agreement.6–10 Intravenous MCE, however, was in its infancy at the time of these studies and was highly susceptible to artefacts. The need for high ultrasound transmission power with a significant tissue background signal resulted in a narrow ratio of myocardial contrast to tissue signal, often preventing unequivocal image interpretation. Intermittent imaging, required to minimise ultrasound induced microbubble destruction, impeded the spatial orientation during echocardiographic visualisation of the myocardium in the apical four and two chamber views. Myocardial contrast echocardiography

Optison (Amersham Health, Oslo, Norway), a second generation ultrasound contrast agent consisting of perfluoropropane filled albumin microspheres (mean diameter 3.9 μm, concentration 5 × 10⁸–8 × 10⁸/ml), was used. For each echocardiographic view, 1 ml of Optison was injected intravenously over 30 seconds through a multidirectional stopcock and 5 ml of 0.9% saline were simultaneously injected to prevent microbubble floating.

An HDI-5500 ultrasound system (ATL Philips Medical Systems, Bothell, Washington, USA) equipped with a...
by consensus. Preceding the SPECT data. Differences in opinion were resolved blinded to both clinical and echocardiographic data interpretation. Two observers blinded to both clinical and SPECT data interpreted analysis of wall motion, MCE, and SPECT (fig 1). Two A 12 segment model of the left ventricle was used for the analysis of wall motion, MCE, and SPECT (fig 1). Two observers blinded to both clinical and echocardiographic data interpreted regional wall motion and MCE. Similarly, two observers blinded to both clinical and echocardiographic data interpreted the SPECT data. Differences in opinion were resolved by consensus.

Wall motion
Regional wall motion was graded as 1, normal; 2, hypokinetic; or 3, akinetic.

MCE
Myocardial opacification in each of the 12 segments was graded as 1, normal; 2, mild reduction; or 3, severe reduction. Reduced myocardial opacification in segments with normal wall motion was assessed as artefact.

SPECT
The horizontal and vertical long axis planes closest to the echocardiographic apical two and four chamber views were used for interpretation. Tracer uptake was assessed in each of the 12 myocardial segments and graded as 1, normal; 2, mild reduction; or 3, severe reduction. Reduced myocardial tracer uptake in segments with normal wall motion was assessed as artefact.

Interobserver and intraobserver variability
Two observers separately scored 20 randomly selected sets of MCE data to determine interobserver variability. After two months, one of the observers repeated the reading and intraobserver variability was calculated.

Statistical analysis
Continuous variables are expressed as mean (SD); nominal variables are expressed as count and percentage. The agreement between MCE and SPECT scores and the interobserver and intraobserver agreement were characterised by κ statistics. Values of > 0.4, > 0.6, and > 0.8 indicate fair, good, and excellent agreement, respectively. Sensitivity and specificity of MCE for detection of regional signal reduction on SPECT were determined. The non-parametric signed rank Kolmogorov-Smirnov test was used to test whether the difference in the number of segments with reduced myocardial signal between MCE and SPECT exceeded one segment. A probability value of p < 0.05 was considered significant.

RESULTS
Patient characteristics
We enrolled 117 patients in the study. For 14 patients, inadequate image quality on MCE prevented meaningful assessment of myocardial opacification. Three patients did not undergo SPECT. Table 1 lists the demographic, clinical, and angiographic characteristics of the 100 patients eligible for image analysis.

Myocardial opacification and wall motion on echocardiography
We used 1064 of 1200 segments (88%) for final comparison. We excluded 66 segments (6%) due to artefacts on MCE (myocardial opacification score 2 or 3 in the presence of normal contraction) and 58 segments (5%) were excluded due to artefacts on SPECT (myocardial uptake score 2 or 3 in the presence of normal contraction). In 12 segments (1%) artefacts were identified both on MCE and on SPECT and these segments were also excluded. On MCE, artefacts mainly occurred in basal segments of the anterior and lateral aspects of the left ventricle.

![Diagram of myocardial segments and coronary perfusion territories of the left anterior descending coronary artery (LAD), left circumflex artery (LCX), and right coronary artery (RCA).](http://heart.bmj.com/)

**Figure 1** Myocardial segments and coronary perfusion territories of the left anterior descending coronary artery (LAD), left circumflex artery (LCX), and right coronary artery (RCA).

1.7 MHz transducer was used. Real time MCE was performed with power pulse inversion imaging. The dynamic range of this system was set to the high level and the frame rate during real time imaging was 15 Hz. Gain settings were optimised at the beginning of each study and held constant throughout. The focus was set at the level of the mitral valve. Mechanical indices between 0.12 and 0.18 were used. Two and four chamber views were stored on S-VHS videotape.

Single photon emission computed tomography
SPECT was performed 45–60 minutes after intravenous injection of 500 MBq of technetium-99m sestamibi. For image acquisition, a dual head rotating camera system (ADAC Vertex Plus, Milpitas, California, USA) with low energy, high resolution collimators was used. In a step and shoot acquisition mode, 32 images were acquired by clockwise eccentric rotation over a 180° arc. Acquisition time of 40 seconds for each image and a 64 × 64 matrix were used. Images were reconstructed with a dedicated software package (Pegasys version 3.4, Pegasys Inc, Tokyo, Japan) and a Butterworth filter (order 5, 0.4 Nyquist cut-off frequency). Tomographic slices reoriented to the short axis and to the vertical and horizontal long axes of the heart were generated. Vertical and horizontal long axis slices corresponding to the echocardiographic two and four chamber views were selected for comparison with MCE.

Image interpretation
A 12 segment model of the left ventricle was used for the analysis of wall motion, MCE, and SPECT (fig 1). Two observers blinded to both clinical and SPECT data interpreted regional wall motion and MCE. Similarly, two observers blinded to both clinical and echocardiographic data interpreted the SPECT data. Differences in opinion were resolved by consensus.

Wall motion
Regional wall motion was graded as 1, normal; 2, hypokinetic; or 3, akinetic.

MCE
Myocardial opacification in each of the 12 segments was graded as 1, normal; 2, mild reduction; or 3, severe reduction. Reduced myocardial opacification in segments with normal wall motion was assessed as artefact.

**Table 1** Patient characteristics

<table>
<thead>
<tr>
<th>Variable</th>
<th>Mean (SD) or Number (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age (years)</td>
<td>63 (12)</td>
</tr>
<tr>
<td>Sex</td>
<td>Women 22 (22%), Men 41 (41%)</td>
</tr>
<tr>
<td>Weight (kg)</td>
<td>79 (13)</td>
</tr>
<tr>
<td>Height (cm)</td>
<td>173 (8)</td>
</tr>
<tr>
<td>History of smoking</td>
<td>Obesity 38 (38%)</td>
</tr>
<tr>
<td>Arterial hypertension</td>
<td>CHF 4 (4%)</td>
</tr>
<tr>
<td>Cholesterolaemia</td>
<td>Diabetes mellitus 16 (16%)</td>
</tr>
<tr>
<td>Infarct related artery</td>
<td>History of smoking 63 (63%)</td>
</tr>
<tr>
<td>LAD 50 (50%)</td>
<td>Obesity 38 (38%)</td>
</tr>
<tr>
<td>RCA 33 (33%)</td>
<td>Diabetes mellitus 16 (16%)</td>
</tr>
<tr>
<td>LCX 17 (17%)</td>
<td>History of smoking 63 (63%)</td>
</tr>
</tbody>
</table>

Data are mean (SD) or number (%).
LAD, left anterior descending coronary artery; LCX, left circumflex coronary artery; RCA, right coronary artery.
wall (34 of 66). On SPECT, artefacts mainly occurred in the inferior wall (34 of 58). Analysis of left anterior descending coronary artery and left circumflex artery perfusion territories was feasible for all patients. For four patients, the perfusion territory of the right coronary artery could not be analysed because of artefacts in both inferior segments.

Figures 2 depicts MCE and SPECT studies of a patient with previous lateral myocardial infarction.

MCE showed normal contractile function and normal myocardial opacification in 638 of 1122 (57%) artefact-free segments on MCE. Myocardial opacification was also normal in 94 (8%) hypokinetic and 13 (1%) akinetic segments. In 377 (34%) segments, myocardial opacification was reduced or absent in conjunction with contractile dysfunction.

Table 2 shows agreement between MCE and SPECT with respect to myocardial signal classification as normal and mildly and severely reduced. The two techniques agreed in 881 of 1064 segments (83%, $\kappa = 0.64$). Concordance was highest (91%, $\kappa = 0.68$) in the mid septal segments and lowest in the basal lateral (70%, $\kappa = 0.39$) and mid inferior (71%, $\kappa = 0.38$) segments. By binary segmental classification as normal (score 1) or abnormal (score 2 or 3), concordance between MCE and SPECT reached 90% ($\kappa = 0.77$).

Table 3 shows concordance between MCE and SPECT for normal (score 1) versus reduced myocardial signal (score 2 or 3) on the coronary perfusion territory level. Agreement was present in 251 of 296 territories (85%, $\kappa = 0.71$).

Myocardial defect size on MCE and SPECT

Figure 3 shows the relation between the number of segments with reduced myocardial signal on MCE and SPECT in each patient. On average, the difference in the number of segments with reduced myocardial signal between MCE and SPECT did not exceed one segment ($p < 0.001$).

Sensitivity and specificity of MCE for the detection of an abnormal segment on SPECT were 87% and 91%, respectively. Sensitivity and specificity of MCE on the perfusion territory level were 93% and 93% for the left anterior descending territory, 73% and 97% for the right coronary artery territory, and 97% and 81% for left circumflex artery territory, respectively.

Observer agreement

Intraobserver and interobserver agreement for differentiation of normal and mildly and severely reduced myocardial opacification on MCE were 94% ($\kappa = 0.84$) and 92% ($\kappa = 0.83$), respectively.

DISCUSSION

The present study for the first time shows that the extent of microvascular damage after mechanical reperfusion of acute myocardial infarction, shown on real time MCE, is closely correlated with infarct size. Real time MCE may therefore allow bedside assessment of infarct extent after mechanical reperfusion of acute myocardial infarction.

Physiology of myocardial perfusion imaged with MCE and SPECT

The myocardial contrast signal on MCE and sestamibi signal on SPECT reflect overlapping but not identical physiological aspects of myocardial perfusion. Myocardial opacification on MCE indicates the presence of microbubbles, pure intravascular tracers, in the myocardial microvasculature. This signal is therefore exclusively related to myocardial blood flow. $^{99m}$Tc-sestamibi, in contrast, diffuses into the extravascular space, passively enters the myocyte, and binds to the negatively charged mitochondrial membrane. The myocardial sestamibi signal on SPECT, therefore, requires not only intact blood flow to the myocardium but also myocardial cell integrity—that is, preserved mitochondrial membrane potential. Thus, the correlation between MCE and SPECT in the present study shows a physiological link between

<table>
<thead>
<tr>
<th>MCE (myocardial opacification)</th>
<th>SPECT (myocardial sestamibi uptake)</th>
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<tbody>
<tr>
<td>Normal</td>
<td>Normal</td>
</tr>
<tr>
<td>Mild reduction</td>
<td>Mild reduction</td>
</tr>
<tr>
<td>Severe reduction</td>
<td>Severe reduction</td>
</tr>
<tr>
<td>Normal</td>
<td>675</td>
</tr>
<tr>
<td>Mild reduction</td>
<td>49</td>
</tr>
<tr>
<td>Severe reduction</td>
<td>15</td>
</tr>
<tr>
<td>Mild reduction</td>
<td>30</td>
</tr>
<tr>
<td>Severe reduction</td>
<td>88</td>
</tr>
<tr>
<td>Severe reduction</td>
<td>41</td>
</tr>
<tr>
<td>Severe reduction</td>
<td>11</td>
</tr>
</tbody>
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microvascular and myocellular damage after mechanical reperfusion of acute myocardial infarction.

The time interval of 10 days after mechanical reperfusion may have contributed to the good correlation between MCE and SPECT, since dynamic signal changes early after reperfusion probably have abated by that time.10

Technical aspects of MCE
In previous clinical studies comparing intravenous MCE with radionuclide imaging, second harmonic8,9,10 and power Doppler imaging8 were used. In the multicentre studies of Marwick et al7 and Binder et al6 sensitivities of MCE for the detection of abnormal segments on SPECT at rest were low and ranged from 46–65% and from 20–39%, respectively, depending on the dose of the contrast agent. Jucquois et al11 obtained the best agreement between SPECT and MCE. In their study, the overall agreement between the techniques was 82% (k = 0.65). Sensitivity and specificity of MCE for the detection of abnormal segments on SPECT were 76% and 83%, respectively. Their study, however, comprised a relatively small number of patients and 26% of all segments could not be used for comparison with SPECT due to artefacts on MCE.

We attribute the improved concordance between MCE and SPECT of the present study to the increased signal to noise ratio of the power pulse inversion technique.12 This assumption is supported by the comparably low rate of uninterpretable segments in the present study. Furthermore, MCE is simplified by the real time feasibility of power pulse inversion technique improving spatial orientation during the examination, which, in its own right, may have contributed to the excellent concordance with SPECT in the present study. After all, the recognition of MCE artefacts is facilitated by the simultaneous assessment of regional myocardial perfusion and wall motion. Disadvantages of power pulse inversion technique, on the other hand, include a limited dynamic range, which may have prevented closer correlation between MCE and SPECT in the present study.

Study limitations
The imaging data were analysed only qualitatively in the present study and more accuracy might have been achieved by signal quantification based on signal intensity thresholds. In contrast with continuous infusion of the contrast agent, bolus administration as used in the present study increases the risk of attenuation artefacts on MCE.

Echocardiographic two or four chamber views may not accurately match horizontal and vertical long axis SPECT planes selected for comparison, which may have resulted in erroneous segmental association between the two techniques.

The applicability of the present data is limited to patients with adequate visualisation of all myocardial segments on the baseline echocardiogram.

Conclusions and clinical prospects
Infarct size is not widely determined after reperfusion of acute myocardial infarction because SPECT imaging is not readily available in most hospitals. The close physiological link between myocardial microvascular and myocellular damage after mechanical reperfusion of acute myocardial infarction, shown in the present study, may help to establish the use of real time MCE for infarct size assessment. Real time MCE has the advantage of being a practicable bedside technique with the potential of wide availability. On the basis of the present data, it appears reasonable to evaluate the role of real time MCE for risk stratification after acute myocardial infarction in future studies. In light of increasing numbers of reperfusion strategies for patients with acute coronary syndromes and existing highly effective treatment modalities, real time MCE may serve as versatile tool for rational and cost effective comparison of efficacy differences between the modalities and may guide the planning of large scale mortality trials.

Authors’ affiliations
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Dr Tousek was supported by a grant from the German Cardiac Society, Düsseldorf, Germany. Dr Orban was supported by a grant from the Czech Cardiac Society, Brno, Czech Republic.

REFERENCES

Figure 3 Number of patients with concordant and discordant spatial extent of reduced myocardial signal intensity.

<table>
<thead>
<tr>
<th>SPECT (myocardial septum uptake)</th>
<th>LAD</th>
<th>RCA</th>
<th>LCX</th>
</tr>
</thead>
<tbody>
<tr>
<td>MCE (myocardial opacification)</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Normal</td>
<td>23</td>
<td>32</td>
<td>52</td>
</tr>
<tr>
<td>Abnormal</td>
<td>8</td>
<td>1</td>
<td>15</td>
</tr>
<tr>
<td>Concordance (k)</td>
<td>85% (0.65)</td>
<td>85% (0.63)</td>
<td>84% (0.67)</td>
</tr>
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</table>

Table 3 Signal comparison between MCE and SPECT by myocardial perfusion territories

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54 year old white woman was admitted with a 10 year history of progressive dyspnoea and exertional hypoxia (oxygen saturation fell from 96% to 77% after two minutes of exercise). The typical clinical stigmata of peritongual erythema/telangiectasias and telangiectasias of both the conjunctivae reflection (panel A) and inner mucosa of the lip were noted. A presumptive diagnosis of hereditary haemorrhagic telangiectasia (Osler-Weber-Rendu syndrome) was made and pulmonary artery catheterisation confirmed a right to left shunt. Pulmonary angiography revealed multiple arterial venous malformations (AVMs) (panel B). On further questioning, the patient described a history of worsening headaches that had been diagnosed as “atypical migraines”. Cerebral angiography confirmed a 1 x 1 x 1 cm compact nidus left occipital lobe AVM (panel C). The patient clinically improved after pulmonary coil embolisation and gamma knife ablation of the cerebral AVM.
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Heart 2005 91: 1568-1572 originally published online March 17, 2005
doi: 10.1136/hrt.2004.057844

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