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Analysis of circadian blood pressure rhythms

Sir,

We read with interest the observation by Davies *et al* (1984; **52**: 93–8) on the circadian rhythm of blood pressure. The authors state that Millar-Craig *et al* reported a second peak of blood pressure in the early evening.¹ We consider that this is not a correct citation, as Millar-Craig *et al* reported that "... blood pressure fell progressively during the day and rose in the early hours of the morning."

Davies *et al* mention the difficulties in quantifying variations in the blood pressure. Some of the basic work on rhythmic blood pressure changes (summarised in²) deals with the problems of recording, reproducibility, and analysis of blood pressure patterns. Using cosinor analysis, first introduced by Halberg *et al*³ might improve the accuracy of analysis. It provides an exact calculation of rhythm variables such as mesor, amplitude, and acrophase of circadian rhythmic changes.^{4–6} It would be interesting to evaluate the carefully documented data of Davies *et al* by cosinor analysis. We wonder whether this method of analysis would confirm the reported two hour difference between the nadir of the paced group and the control group.

The authors also point out that the amplitude of the circadian pattern was lower in the paced than in the hypertensive group. Judging from the data in Fig. 1 of their article this seems not unlikely. Quantitative evaluation of the amplitudes, however, is not reported but might be done by cosinor analysis. Furthermore, cosinor analysis might allow a better comparison of circadian heart rate and blood pressure variations.

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This letter was shown to the authors, who reply as follows:

Sir,

We thank Drs Gerbes *et al* for their interest in our paper on circadian rhythms of blood pressure in paced patients. They correctly cite our original description of the broad 24 hour pattern of blood pressure¹; however, most of our data on closer inspection showed a subsidiary late afternoon rise of lower amplitude than that seen after waking. This is visible in Figs. 1 and 3 of the original publication.¹

The problems inherent in describing ambulatory intra-arterial blood pressure patterns have been recognised by several groups of workers. We find it difficult to accept that Halberg's cosinor analysis would be able to provide sufficient accuracy in this case. As we understand it, the technique consists of fitting a single 24 hour cosine curve to the data using the method of least squares. Variables such as the amplitude, mesor (average value), and acrophase (tim-

ing of the peak relative to an arbitrary time origin) are then measured from the fitted curve. The pattern of blood pressure is not symmetrical within a 24 hour cycle; for example, a single cosine function would be a very poor fit to the systolic data in Fig. 1 of our paper. This observation appears to be confirmed by the work of Murnaghan *et al* in their study of blood pressure in pregnancy.² The single cosinor technique failed to give sufficient resolution to describe other than gross features of the blood pressure patterns. Walsh and Goldberg also found that significant components were present at higher frequencies.³ Detailed studies by Sayers⁴ indicate the presence of several concurrent patterns, posing severe problems in any detailed statistical analysis across patients. More recently, the same group has suggested a set of procedures for pattern analysis of these records, relying more on measurements from each record than on a priori models.⁵ These procedures are at present being applied to blood pressure data from a variety of sources.

In active untreated subjects the timing of the acrophase must be heavily dependent on the time of waking since this is the event which has the greatest effect on blood pressure. This would tend to place the acrophase at approximately 14 hours before waking—that is, at 1800 or so, and this has been the finding of several workers.^{3,6} It is hard to see how this would provide any illumination of our observed shifts in the nadir of blood pressure at around 0100–0300. For critical studies we now compile our data relative to waking time as well as to absolute clock time.

We are therefore unconvinced that cosinor analysis would clarify our observations of ambulatory intra-

arterial blood pressure unless applied in a complex form taking account of many pattern features and frequencies, in which case conventional Fourier analysis seems to offer more possibilities.

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Delayed recovery of left ventricular function after anti-thyroid treatment

Sir,

Forfar *et al* (1984; 52: 215–22) suggest that in hyperthyroidism left ventricular function is reversibly depressed. Their conclusions are based on haemodynamic measurements performed on 15 hyperthyroid subjects before and during isometric exercise, and those measurements were repeated after the subjects had been rendered euthyroid. The authors stress that hyperthyroidism involves changes intrinsic not only to the heart itself but also to the peripheral circulation. They assume, however, that the performance of a standardised isometric exercise task produced the same changes in the peripheral circulation in both hyperthyroid and euthyroid states and, therefore, that exercise caused the same changes in cardiac loading before and after the subjects had

been treated for their thyrotoxicosis. Nevertheless, as shown in the Table below, using data taken from their own paper it may be calculated that isometric exercise actually caused directionally opposite changes in peripheral vascular resistance during the thyrotoxic and euthyroid states. Peripheral vascular resistance is a major determinant of the impedance offered to the outflow of blood from the left ventricle. In the study of Forfar *et al* the thyrotoxic heart, faced with an increased peripheral resistance during isometric exercise, did not function as well as it did at rest. In contrast, the euthyroid heart experienced a large reduction in calculated peripheral vascular resistance during isometric exercise and showed no deterioration in function.

Thus it would appear that peripheral resistance is