included: atrial inhibited (AAI); ventricular inhibited (VVI-RV); dual chamber (DDD-RV); biventricular (DDD-BiV) and left ventricular pacing (DDD-LV). Base rate for pacing was set at 86/min and continued for the duration of level 3 care. The haemodynamic data were measured using a pulmonary arterial catheter using either thermodilution or continuous cardiac output measurements.

Results The baseline demographics are illustrated in Abstract 002 table 1. The acute haemodynamic measurements at 18 h, Abstract 002 table 2.

Abstract 002 Table 1

Demographic	Biventricular pacing	Standard pacing	p Value
Age/years (SD)	69.2 (9.3)	65.5 (12.7)	0.32
Male gender/%	79	79	1.0
NYHA score pre-operation (SD)	2.5 (0.7)	2.4 (0.9)	0.69
Euroscore/additive (SD)	8.3 (3.1)	7 (2.8)	0.18
QRS duration/ms (SD)	113.3 (29.3)	115.2 (24.4)	0.84
CABG only/%	63	58	0.63
Ejection fraction (pre-op)/% (SD)	26.1 (5.4)	28.0 (7.3)	0.34
Cardiopulmonary bypass time/min (SD)	127.1 (41.1)	144 (45.9)	0.25
Duration of Level 3 Care/hours (SD)	44.5 (36.8)	57.1 (73.0)	0.56

Abstract 002 Table 2

Pacing mode	Cardiac output l/min/(SD)	p Value (paired student t test vs AAI)
AAI	5.4 (1.1)	
VVI	4.3 (1.7)	<0.001
DDD-RV	5.3 (1.1)	0.77
DDD-BIV	5.8 (1.2)	0.02
DDD-LV	5.4 (0.7)	0.73

Conclusions BiV pacing significantly improved haemodynamics in the early part of the post-operative period compared to standard AAI pacing at 18 h. There is a suggestion that the improvement in haemodynamic function may translate into clinical benefit. The duration of level 3 care was 57.1 h in the standard pacing group compared to 44.5 h in the BiV group. However, the 22% reduction in level 3 care in the BiV group compared to the standard pacing group did not reach statistical significance.

003 VALIDATING MARKERS OF MECHANICAL DYSSYNCHRONY BY EXPERIMENTAL MANIPULATION OF INTERVENTRICULAR TIMINGS: WHAT IS NEEDED TO MAKE THEM A REASONABLE PROSPECT FOR CARDIAC RESYNCHRONISATION THERAPY SELECTION?

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Background Any dyssynchrony marker proposed for selection of patients for cardiac resynchronisation therapy (CRT) should be stable between heartbeats but change markedly when interventricular delay is experimentally manipulated; the marker should also minimise at some "optimal" interventricular delay.

Methods and Results We performed 3264 echocardiographic measurements in 13 patients with CRT: separate, replicate measurements at interventricular delays from RV-first 40 ms to LV-first 60 ms, in 20-ms intervals of (1) 3D systolic dyssynchrony index (SDI), (2) Tissue Doppler imaging (TDI), (3) aortic pre-ejection time, (4)

interventricular mechanical delay (IVMD), (5) LVOT VTI and (6) QRS duration. In each patient, we identified with blinding on several successive repetitions, an apparently-optimal (minimally-dyssynchronous) interventricular delay for each variable. Agreement between successive optimisations was low: κ values of 0.24 for SDI, 0.02 for TDI, 0.36 for aortic pre-ejection time, 0.14 for IVMD, 0.40 for LVOT VTI and 0.47 for QRS duration. Intraclass correlation coefficient, indicating measurement reproducibility, was low when single measurements were taken (ranging across methods from 0.32 to 0.63), but improved when pairs of measurements were averaged (0.51 to 0.74, $p=0.0008$). Using averages of pairs of measurements reduced the disagreement between replicate optimisations $p=0.007$.

Conclusions Under blinded conditions these mechanical dyssynchrony markers cannot reliably discriminate even large changes in interventricular delay, and can be quickly rejected as candidates for predicting clinical benefit from CRT. It would save time and expense if markers considered for clinical trialling under formal scientific conditions first underwent screening for plausibility by such a stage of inexpensive, active experimentation.

004 SIMULTANEOUS INVASIVE PRESSURE AND FLOW MEASUREMENTS DURING ATRIOVENTRICULAR DELAY IMPROVEMENT REVEAL A COMPENSATORY PERIPHERAL VASODILATOR RESPONSE WHICH ATTENUATES THE INITIAL BLOOD PRESSURE INCREMENT: IMPLICATIONS FOR THE DESIGN OF OPTIMISATION PROTOCOLS

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Introduction With synchrony of ventricular contraction already restored by cardiac resynchronisation therapy (CRT), optimisation of atrioventricular (AV) delay relies on improving filling. Although when AV delay is improved blood pressure immediately rises, there is a subsequent partial decline. Is this secondary decline because (1) non-invasive measurements are unreliable, (2) cardiac function increment is short-lived or (3) peripheral vasodilatation occurs? We conducted invasive experiments to distinguish between these hypotheses.

Methods Nine patients with heart failure and CRT underwent changes in programmed AV delay from 40 ms to 120 ms. We simultaneously measured beat-by-beat invasive aortic pressure and flow, and non-invasive pressure (Finometer). Triplicate sets of experiments were performed and averaged to minimise the impact of noise.

Results There was an immediate increment in invasive blood pressure of $+14.7 \pm 2.0$ mm Hg ($p=0.0001$), but after ~ 10 beats there

Abstract 004 Figure 1

was a secondary progressive decline to a lower plateau of $+8.0 \pm 1.8$ mm Hg ($p=0.004$), Abstract 004 figure 1. The initial increment was caused by an immediate rise in flow by $+9.1 \pm 2.4\%$ ($p=0.007$) which did not drop later. The secondary decline in pressure was caused by a delayed gradual decline in total peripheral resistance. Finometer-derived non-invasive blood pressure tracked invasive pressure closely ($r=0.97$).

Conclusion When AV delay is made more favourable, only the instant pressure increment is caused by increase in stroke volume. The secondary pressure decline is caused by systemic vasodilatation. Design of AV optimisation protocols, which face severe challenge of signal vs noise, might benefit from recognition that not all beats are equally informative: the first few after a transition are most signal-rich.

005 CARDIAC MRI: UNDERSTANDING MYOCARDIAL MOTION TO PREDICT REMODELLING PRE CARDIAC RESYNCHRONISATION THERAPY

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Introduction A significant number of patients undergoing Cardiac Resynchronisation Therapy (CRT) do not remodel. Assessing global dyssynchrony has the potential to improve patient selection. We developed a framework for comparing measures of myocardial motion from cardiac magnetic resonance (CMR) imaging and evaluated the potential of these techniques to improve patient selection.

Methods 48 patients recruited, (43 males, 63.8 ± 13.9 years), NYHA class 2.9 ± 0.5 , ejection fraction $25 \pm 9\%$. Patients had LBBB (QRS 154 ± 24 ms). Acute haemodynamic response was measured at time of implant with a pressure wire in the LV measuring change in dp/dt_{max} . A $>10\%$ increase in LV- dp/dt_{max} from baseline was considered an acute response. Decrease in end systolic volume (ESV) $\geq 15\%$ at 6 months was used to determine remodelling. CMR was performed prior to CRT. A novel framework was developed. Key steps included: (1) detection of heart and myocardium segmentation from anatomical CMR cine images; (2) detection of endo and epi-cardial surfaces for wall thickening computation; (3) extraction of deformation fields within the myocardium for strain computation. A systolic dyssynchrony index (SDI) was produced for all parameters

Abstract 005 Figure 1 Shows the ANOVA plots for acute response and remodelling for QRS duration, volume and muscle thickening derived SDI.

which included volume change, muscle thickening, radial, circumferential, longitudinal strain and combined strain. High SDI denoted dyssynchrony. Results Pre-implant ESV 175 ± 64 ml, post-implant ESV 155 ± 68 ml ($p<0.01$). 20 (44%) patients remodelled. We found a strong relationship between volume derived SDI and acute response ($p=0.008$) and remodelling ($p<0.001$) (Abstract 005 figure 1). We found a weaker relationship with remodelling and muscle thickening SDI ($p=0.001$) and no relationship with a SDI derived from strain indexes (Abstract 005 figure 2). Volume SDI $\geq 10\%$ was highly sensitive (0.94) and specific (0.87) for predicting remodelling. Volume SDI was far superior for predicting remodelling than any other method. The intra-observer average difference for volume SDI

Abstract 005 Figure 2 Shows the ANOVA plots for acute response (top row) and remodelling (bottom row) for SDI derived from various types of strain.