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Original research

Smartphone detection of atrial fibrillation using photoplethysmography: a systematic review and meta-analysis

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► Additional supplemental material is published online only. To view, please visit the journal online (<http://dx.doi.org/10.1136/heartjnl-2021-320417>).

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Received 9 October 2021
Accepted 24 January 2022
Published Online First
11 March 2022

ABSTRACT

Objectives Timely diagnosis of atrial fibrillation (AF) is essential to reduce complications from this increasingly common condition. We sought to assess the diagnostic accuracy of smartphone camera photoplethysmography (PPG) compared with conventional electrocardiogram (ECG) for AF detection.

Methods This is a systematic review of MEDLINE, EMBASE and Cochrane (1980–December 2020), including any study or abstract, where smartphone PPG was compared with a reference ECG (1, 3 or 12-lead). Random effects meta-analysis was performed to pool sensitivity/specificity and identify publication bias, with study quality assessed using the QUADAS-2 (Quality Assessment of Diagnostic Accuracy Studies-2) risk of bias tool.

Results 28 studies were included (10 full-text publications and 18 abstracts), providing 31 comparisons of smartphone PPG versus ECG for AF detection. 11 404 participants were included (2950 in AF), with most studies being small and based in secondary care. Sensitivity and specificity for AF detection were high, ranging from 81% to 100%, and from 85% to 100%, respectively. 20 comparisons from 17 studies were meta-analysed, including 6891 participants (2299 with AF); the pooled sensitivity was 94% (95% CI 92% to 95%) and specificity 97% (96%–98%), with substantial heterogeneity ($p < 0.01$). Studies were of poor quality overall and none met all the QUADAS-2 criteria, with particular issues regarding selection bias and the potential for publication bias.

Conclusion PPG provides a non-invasive, patient-led screening tool for AF. However, current evidence is limited to small, biased, low-quality studies with unrealistically high sensitivity and specificity. Further studies are needed, preferably independent from manufacturers, in order to advise clinicians on the true value of PPG technology for AF detection.

heart failure and cognitive decline. In particular, there is a fivefold increased risk of stroke, where at the time of stroke, up to a third of patients either have a known or new diagnosis of AF. These strokes tend to be more disabling when compared with strokes from other causes, and are largely preventable with oral anticoagulation.^{2–4} According to the European Society of Cardiology guidelines, patients aged over 65 years can benefit from AF screening using single timepoint, repeated or ambulatory electrocardiogram (ECG) recordings.⁴ However, there is a risk of missing paroxysmal episodes as AF can be brief and sporadic. This was seen in the STROKESTOP study (systematic ECG screening for AF among 75-year-old subjects), where short intermittent home ECG recordings resulted in higher sensitivity rates for the detection of new AF compared with one-off measurement.⁵

The development of novel screening devices has the potential to increase screening coverage and improve clinical detection of AF. Smartphone applications can allow self-detection of arrhythmias, allowing for patient self-care and involvement.⁶ Photoplethysmography (PPG) technology found in smartphone cameras can be used for AF screening by patients in the community. The technique uses the light-emitting diode in cameras to measure pulsatile changes in light intensity that are reflected from a finger (or face). Several smartphone PPG applications are currently available, but their clinical value for AF detection is unclear. The majority are commercial products, and there is justified concern over publication bias.⁷ In this systematic review, we assess the diagnostic accuracy of AF detection using smartphone PPG applications in comparison to a gold-standard ECG recording and provide guidance to clinicians about the value and limitations of their potential use to guide clinical management.

INTRODUCTION

Atrial fibrillation (AF) is the most common cardiac arrhythmia encountered by healthcare professionals with rising prevalence, particularly in older patients and those with predisposing comorbidities.¹ Timely identification is key due to the significant impact that AF has on patient quality of life and mortality, in addition to morbidity due to thromboembolism,

METHODS

Eligibility and search strategy

This review was conducted according to the Preferred Reporting Items for Systematic Reviews and Meta-Analyses (PRISMA) guidelines and was prospectively registered with the PROSPERO database of systematic reviews (registration number: CRD42019109455). A systematic review



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To cite: Gill S, Bunting KV, Sartini C, et al. *Heart* 2022;**108**:1600–1607.

of MEDLINE (1950–1 December 2020), EMBASE (1980–1 December 2020), and the Cochrane Library (until 1 December 2020) was performed without language restriction (see online supplemental tables S1 and S2 for search terms). We also manually searched reference lists of relevant studies for any further available literature.

Inclusion and exclusion criteria

All publications examining any type of AF were evaluated (paroxysmal, persistent or permanent as defined by the study), including original research and conference abstracts in participants aged 18 years and above. We required (1) comparison with a reference standard ECG (1, 3 or 12-lead); and (2) AF detection using a smartphone camera to analyse the PPG signal from a fingertip or the face. Editorials and reviews were excluded, in addition to publications that did not meet the study objectives. For example, we excluded use of wrist-worn devices to generate PPG signals (as these require additional hardware beyond a smartphone) and studies that lacked a reference ECG.

Outcomes

The outcomes considered were validation of AF detection by examining (1) sensitivity; (2) specificity; (3) positive predictive value (PPV); (4) negative predictive value (NPV); and (5) overall accuracy.

Data extraction

All publications that were identified from literature searches were initially screened based on title and abstract by two independent reviewers (SG and KVB). Data were stored in a standardised tabular format and the full list was assessed for eligibility by two different reviewers independently. Following screening, any discrepancies were discussed between the reviewers (SG, KVB).

Any further conflicts were resolved by reviewing the original publication and additional adjudication.

Two reviewers (SG and KVB) assessed the full text of each article or abstract with four evidence-based hierarchy criteria: (1) original research reporting findings for all outcomes considered; (2) original research reporting findings for some, but not all, outcomes; (3) conference abstract reporting findings for all outcomes; (4) conference abstract reporting findings for some, but not all, outcomes. During the assessment, publications meeting the criteria above were extracted at study level, and a table was generated including relevant information (the disease of interest, setting, population and sample size, type of smartphone application, outcomes measured, reference test and study quality results). We sought additional data on missing parameters from lead authors of the publications included, but no additional data were received. Where relevant, we made note of industry involvement in the study (eg, study funding, authors employed in industry and provision of study devices or technology).

Risk of bias

All studies were assessed by two independent reviewers (SG and KVB) using the Quality Assessment of Diagnostic Accuracy Studies-2 (QUADAS-2) tool.⁸ This assesses four key domains: (1) patient selection; (2) index test used (smartphone application for AF detection via fingertip or facial PPG signal); (3) reference standard used (1, 3 or 12-lead ECG); and (4) flow and timing. All domains were assessed for risk of bias using signalling questions, and the first three for applicability to the review question. Each domain is given a score of high, low or unclear for risk of bias and applicability.

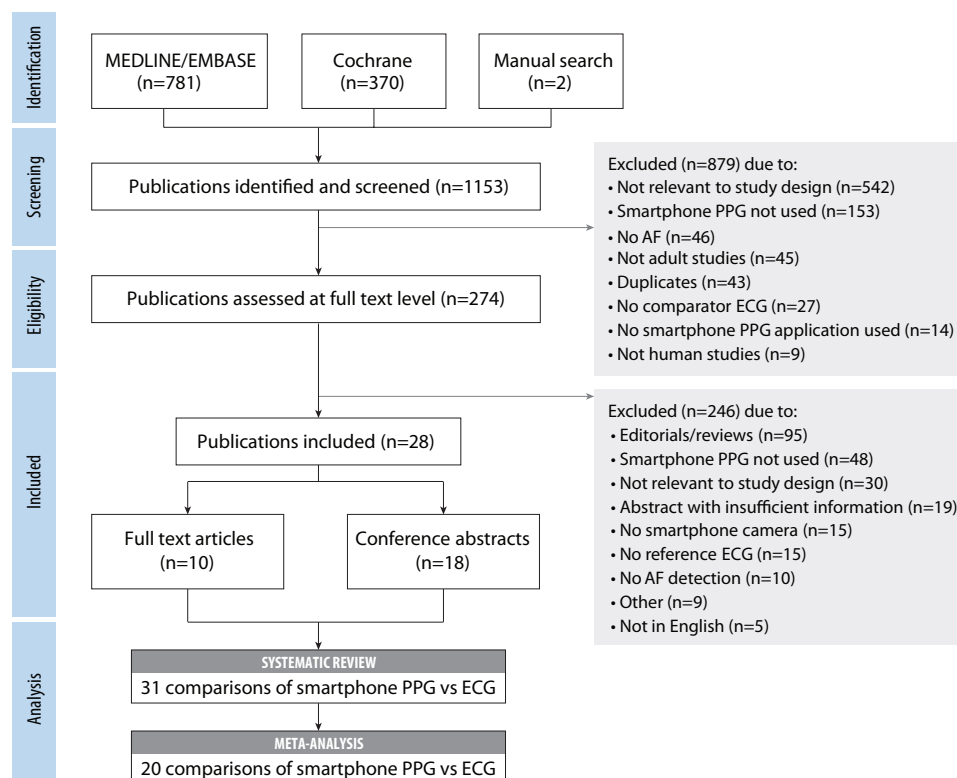


Figure 1 Flow diagram for systematic review. Flowchart demonstrating selection of eligible studies. AF, atrial fibrillation; ECG, electrocardiogram; PPG, photoplethysmography.

Table 1 Summary of full-text studies

Study	Study design and key enrolment criteria	Setting and sample size	Population characteristics	Technology for AF detection	Reference test
Brasier <i>et al</i> 2019 ³⁰	Prospective, multicentre Age >18 years, capable of written consent Supported by industry	Secondary care N=672 AF prevalence 42%	Age 78 years (median); female 45%; hypertension 72%; diabetes 31%; heart failure 36%; stroke 16%; OAC 49%	iPhone 4S; Preventicus app; 300 s recording; data quality check performed prior to rhythm analysis that used beat-to-beat changes of pulse wave time intervals and morphology	Blinded interpretation of single-lead ECG by two cardiologists with group consensus; three study comparisons with PPG signal analysed at (1) 60 s; (2) 120 s; and (3) 300 s.
Chan <i>et al</i> 2016 ¹¹	Prospective, single centre Age ≥65, history of hypertension, diabetes Supported by industry	Primary care, N=1013 AF prevalence 3%	Age 68 years (mean); female 53%; hypertension 90%; diabetes 37%; heart failure 4%; stroke 11%	iPhone 4S; CRMA app; 3×17 s recordings, baseline wander and noise filtered. AF detection based on a lack of repeating patterns in the PPG waveform, using SVM. Labelled AF if 2 of 3 recordings irregular.	Blinded interpretation of single-lead ECG by two cardiologists with group consensus.
Fan <i>et al</i> 2019 ¹²	Prospective, single centre Age >18 years Excluded if unable to use smartphone or had memory impairment Supported by industry	Secondary care n=108 AF prevalence 48%	Female 42%; diabetes 30%; heart failure 13%; stroke 12%; OAC 46%	Huawei Mate 9, Huawei Honor 7X; Preventicus app; 180-second recording analysed	12-lead ECG interpreted by two cardiologists with group consensus.
McManus <i>et al</i> 2013 ¹³	Prospective single centre AF for DCCV	Secondary care N=76 AF prevalence 100%	Age 65 years (mean); female 35%; hypertension 71%; diabetes 28%; heart failure 21%; stroke 12%	iPhone 4S; unknown app; 120 s recording, analysed using two statistical techniques (RMSSD and ShE)	12-lead ECG interpreted by trained physicians with group consensus.
McManus <i>et al</i> 2016 ¹⁴	Prospective single centre AF for DCCV and premature beats	Secondary care, N=121 AF prevalence 81%	Age 66 years (mean); female 18%	iPhone 4S; PULSESART app; 120 s recording analysed using three statistical techniques (RMSSD, ShE, Poincaré plot)	12 or 3-lead ECG, interpreted by trained physicians with group consensus.
Mutke <i>et al</i> 2020 ³¹	Prospective, multicentre; data from two trials (WATCH AF and DETECT PRO) Supported by industry	Secondary care N=1330 AF prevalence 47%		iPhone 4S; Preventicus app; 60 s recording analysed using beat-to-beat variations via a non-linear rhythm analysis, signal quality check not performed	Single-lead ECG. Interpretation by two cardiologists with group consensus.
Poh <i>et al</i> 2018 ³⁶	Retrospective analysis with DCNN for AF detection Supported by industry	Validation data from primary care N=1013 AF prevalence 3%	Age 68 years (mean); female 53%; hypertension 90%; diabetes 37%; stroke 11%; heart failure 4%	iPhone4S; unknown app; 3×17 s recordings analysed using six AF detection algorithms (CoV, 5 CoSEn, nRMSSD +ShE, RMSSD +SD1/SD2, Poincaré plot and SVM)	Blinded interpretation of single-lead ECG by two cardiologists with group consensus.
Proesmans <i>et al</i> 2019 ³²	Prospective multicentre Age ≥65 years, paroxysmal or persistent AF Supported by industry	Primary care N=223 AF prevalence 46%	Age 77 years (mean); female 53%; diabetes 20%; heart failure 29%; stroke 22%; OAC 56%	iPhone 5S; Fibrichk app; 3×60 s recordings; signal quality evaluated using RR-interval variability analysis; AF detection based on recurrent neural network algorithm	Blinded 12-lead ECG interpretation by two cardiologists with group consensus.
Rozen <i>et al</i> 2018 ¹⁵	Prospective single centre Age >18 years, AF for DCCV Supported by industry	Secondary care N=97 AF prevalence 90%	Age 68 years (mean); female 25%	iPhone; CRMA app; 3×20 s recordings analysed using SVM to classify PPG waveforms; feature extraction used to determine self-similarity of waveform; labelled AF if at least 2 of the three recordings irregular	Blinded 12-lead ECG interpretation by two cardiologists with group consensus.
Yan <i>et al</i> 2018 ¹⁶	Prospective single centre Supported by industry	Secondary care; N=233 AF prevalence 35%	Age 70 years (mean); female 30%; hypertension 60%; diabetes 35%; heart failure 32%; stroke 19%	iPhone 6S; CRMA app; 3×20 s recordings, baseline wander and noise filtered; AF detection using SVM (based on lack of repeating patterns); AF if irregular in ≥1, or three consecutive uninterpretable measurements	Blinded interpretation by cardiologist of 12-lead ECG; two study comparisons of (1) facial PPG and (2) finger PPG.

See online supplemental table S1 for summary of conference abstracts.

AF, atrial fibrillation; CoSEn, coefficient of sample entropy; CoV, coefficient of variation; CRMA, cardio rhythm smartphone application; DCCV, direct current cardioversion; DCNN, deep convolutional neural network; ECG, electrocardiogram; OAC, oral anticoagulation; PPG, photoplethysmography; RMSSD, root mean square of successive RR differences; ShE, Shannon entropy; SVE, support vector machine.

Patient and public involvement (PPI)

A PPI team were not involved in the design, conduct, reporting or dissemination plans of our research.

Ethics

This study follows the principles of the World Medical Association's Declaration of Helsinki. In this case, separate ethical

Table 2 Characteristics of participants

Characteristic	Number of studies providing data	Weighted mean (SD) or n (%)	Minimum	Maximum
Age, years	15	67 (SD 4.9)	59	77
Women	18	709 (48%)	18%	59%
Prevalence of AF	26	2422 (31%)	0.5%	100%
Hypertension	7	527 (83%)	59%	90%
Diabetes	8	239 (33%)	20%	37%
Stroke	8	125 (14%)	11%	23%
Heart failure	8	170 (16%)	4%	38%

AF, atrial fibrillation.

approval was not required as the study is a meta-analysis of previously published tabular information from relevant studies.

Statistical analysis

All results for sensitivity, specificity, PPV, NPV and diagnostic accuracy for smartphone AF detection were visualised using forest plots. When not directly reported by study authors, we derived diagnostic values using 2×2 contingency tables from reported sensitivity, specificity and corresponding confidence intervals. Due to uncertainty in the number of patients with AF, we were unable to produce a contingency table for one study.⁹ Publication bias was assessed using a funnel plot of linear regression of the log ORs on the inverse root of the sample size, with asymmetry and/or a non-zero slope coefficient with $p<0.1$

indicative of small study bias. Bivariate mixed-effects regression modelling was used to meta-analyse study comparisons with confidence intervals for sensitivity and specificity. A summary receiver operating characteristic plot was constructed to provide information on the overall diagnostic accuracy of smartphones for AF detection with 95% prediction regions. Heterogeneity was assessed using the I^2 statistic, and visually using the bivariate box plot approach. Statistical analysis was performed using Stata V.14.2 (StataCorp LP, Texas, USA) and the MIDAS program.¹⁰

RESULTS

The search strategy identified a total of 1153 publications (figure 1), of which 28 studies were included in the systematic review. Ten studies were full-text original research publications and 18 were conference abstracts.

Design, devices and population

Of the 28 studies included, 25 were prospective, of which 19 were conducted in a single centre^{9 11–29} and 6 involved two or more centres.^{23 30–34} Sixteen studies were conducted in secondary care,^{9 12–20 22 25 26 29–31} seven in primary care,^{11 21 23 24 32–34} three were unspecified^{27 28 35} and three used retrospective databases.^{35 36} Nine studies conducted in secondary care included those with known AF scheduled for cardioversion or catheter ablation.^{9 13–15 19 20 22 25 26} Details on inclusion and exclusion criteria for each study are presented in table 1 (and online supplemental table S3 for conference abstracts).

In terms of devices, 16 studies used an Apple iOS smartphone,^{9 11 13–16 18–20 26 29–32 36} 1 study used an Android

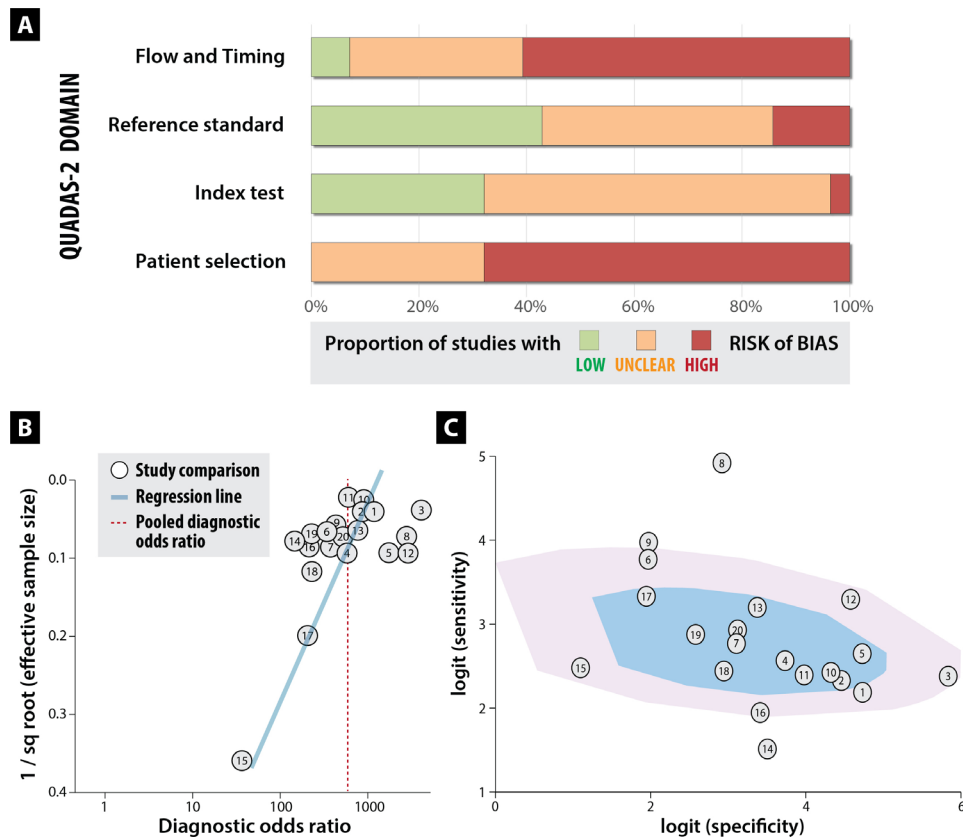


Figure 2 Risk of bias, publication bias and heterogeneity. Top panel (A; bar chart) shows the overall risk of bias based on QUADAS-2 criteria (see online supplemental table S4 for each study). Bottom panel demonstrates high likelihood of publication bias (B; weighted funnel plot) and study heterogeneity (C; bivariate box plot with the inner shaded area representing the median distribution of sensitivity and specificity, and the outer area the 95% confidence bound). See table 3 for numbers linking to each study comparison.

Table 3 Summary of sensitivity, specificity and accuracy of PPG

Study (comparison)	Meta-analysis comparison number	Sensitivity % (95% CI)	Specificity % (95% CI)	PPV % (95% CI)	NPV % (95% CI)	Accuracy % (95% CI)
Brasier <i>et al</i> 2019a ³⁰	1	90 (86 to 93)	99 (98 to 100)			89
Brasier <i>et al</i> 2019b ³⁰	2	91 (87 to 95)	99 (97 to 100)			78
Brasier <i>et al</i> 2019c ³⁰	3	92 (86 to 95)	100 (98 to 100)			61
Chan <i>et al</i> 2016 ¹¹	4	93 (77 to 99)	98 (97 to 99)	54 (38 to 68)	100 (99 to 100)	
Fan <i>et al</i> 2019 ¹²	5	95 (92 to 97)	100 (98 to 100)	100 (98 to 100)	96 (93 to 98)	98 (96 to 99)
Grieten <i>et al</i> 2018–1 ³³	6	98 (92 to 100)	88 (80 to 94)	88 (82 to 93)	98 (92 to 99)	
Grieten <i>et al</i> 2018–2 ³⁴		100	97			
Karim <i>et al</i> 2017 ¹⁷	7	94 (85 to 98)	96 (87 to 99)			
Kuan <i>et al</i> 2018 ¹⁸ *	8	100 (83 to 100)	95 (84 to 99)			
Maitas <i>et al</i> 2012–1 ²⁰		100	99			99
Maitas <i>et al</i> 2012–2 ¹⁹		96	100			98
McManus <i>et al</i> 2013 ¹³		96	98			97
McManus <i>et al</i> 2016 ¹⁴		97	94			95
Mortelmans <i>et al</i> 2017 ²¹	9	98 (92 to 100)	88 (80 to 94)			93 (89 to 96)
Mukte <i>et al</i> 2019 ³⁵	10	92 (89 to 94)	99 (97 to 99)	98 (92 to 96)	94 (92 to 96)	
Mutke <i>et al</i> 2020 ³¹	11	92 (89 to 94)	98 (97 to 99)			95
Napolitano 2015		97	94			95
Poh <i>et al</i> 2018 ³⁶	12	95 (88 to 99)	99 (98.6 to 99.3)	73 (65 to 79)	100 (100 to 100)	
Proesmans <i>et al</i> 2019–1 ³²	13	96 (89 to 99)	97 (91 to 99)	63 (61 to 65)	100 (100 to 100)	
Proesmans <i>et al</i> 2019–2 ²²	14	81 (76 to 86)	97 (96 to 98)	95 (94 to 96)	89 (87 to 91)	91 (89 to 93)
Proesmans <i>et al</i> 2018 ²³		100	97			97
Rozen <i>et al</i> 2018 ¹⁵	15	93 (87 to 97)	91 (83 to 96)	92 (86 to 96)	92	92
Rozen <i>et al</i> 2017 ⁹		96 (90 to 99)	93 (87 to 97)	93 (86 to 97)	96 (90 to 99)	96
Siu <i>et al</i> 2016 ²⁴		93	98			
Smeets <i>et al</i> 2019 ²⁵	16	88 (85 to 91)	97 (94 to 100)	98 (97 to 99)	77 (72 to 82)	90 (88 to 92)
Vaid <i>et al</i> 2015 ²⁶	17	97 (82 to 100)	85 (69 to 94)	83 (67 to 93)	97 (83 to 100)	
Vandenberk <i>et al</i> 2018–1 ²⁸		97	99			
Vandenberk <i>et al</i> 2018–2 ²⁷		82	93	92	84	
Yan <i>et al</i> 2016 ²⁹	18	93 (77 to 98)	95 (86 to 98)			
Yan <i>et al</i> 2018a ¹⁶	19	95 (87 to 98)	96 (91 to 98)	92 (84 to 96)	97 (93 to 99)	95
Yan <i>et al</i> 2018b ¹⁶	20	95 (87 to 98)	93 (88 to 96)	88 (80 to 93)	97 (93 to 99)	94

See table 1 for details of comparisons within studies.

smartphone,¹² a further 2 studies used a combination^{22 25} and 9 studies did not specify the smartphone used.^{17 21 23 24 27 28 33–35} The most common PPG applications used were Cardiio Rhythm mobile application (CRMA; eight studies), Fibrichk (four studies), Preventicus (five studies) and PULSESMART (two studies), with nine studies not specifying the application.^{13 19 20 22 23 25 36} A 12-lead ECG was used as a reference standard in 13 studies, while 11 studies used a single-lead ECG and 4 studies used a combination of 12-lead, single or 3-lead ECG. Only three studies documented performing the PPG and ECG recording simultaneously.^{12 27 35}

The total number of participants was 11 404, of which 2422 (21.2%) had an ECG diagnosis of AF. The prevalence of AF varied from 0.5% to 100% in individual studies. The average age (where stated) ranged from 59 to 77 years, with a weighted mean of 67 years (SD 4.9). The proportion of women ranged from 18% to 59%, with a weighted average of 48.2% (table 2).

Risk of bias and publication bias

The included studies were found to be of low quality overall; none were graded as meeting all QUADAS-2 criteria. Levels of bias were consistent across full-text studies (online supplemental table S4) and abstract-only studies (online supplemental table S5), even though assessment of the latter was limited by shorter

description. The major concerns related to high risk of bias, particularly for patient selection (eg, selection of non-random patients), and the conduct of the study (exclusion of data from final analysis and unclear timing of reference and index tests) (figure 2A). Regression of effect size on sample size demonstrated a non-zero slope coefficient across comparisons with asymmetry (figure 2B). After excluding the largest study, the p value for the slope coefficient was 0.06 (p<0.10 suggestive of small study/publication bias). Heterogeneity is visualised on the bivariate box plot, with a number of studies outside the fence area (figure 2C).

Detection of AF

The 28 studies included provided 31 comparisons for AF detection using PPG smartphone applications against conventional ECG (29 fingertip and 2 facial PPG). A comparative summary by study is presented in table 3, and by smartphone PPG application online in online supplemental table S6. Sensitivity ranged from 81% to 100%, specificity from 85% to 100%, PPV 54% to 100% and NPV 77% to 100% (online supplemental figures S1 and S2). Accuracy was reported in 18 comparisons and ranged from 61% to 99%.

In meta-analysis of 20 comparisons of AF detection from 17 studies (n=5561; 1674 with AF), the pooled sensitivity was

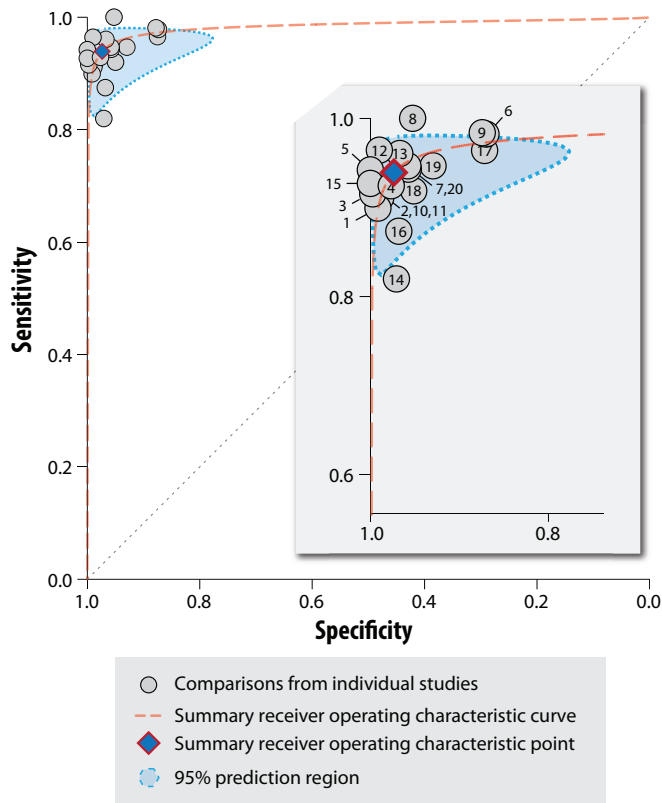


Figure 3 Summary receiver operator characteristic plot. Includes all comparisons in the meta-analysis (see table 3 for numbers linking to each study comparison) with summary receiver operator characteristics. Note that significant heterogeneity was identified across studies overall ($p < 0.0001$), and for sensitivity and specificity individually ($I^2 = 49.6\%$; $p = 0.01$ and $I^2 = 85.3\%$; $p < 0.01$).

94% (95% CI 92% to 95%), with significant heterogeneity ($I^2 = 49.6\%$; $p = 0.01$). The pooled specificity was 97% (95% CI 96% to 98%), with significant heterogeneity ($I^2 = 85.3\%$; $p < 0.01$). Overall, the area under the receiver operating curve was 0.98 (95% CI 0.97 to 0.99), again with substantial significant heterogeneity ($I^2 = 98\%$; $p < 0.0001$) (figure 3).

DISCUSSION

This systematic review has identified the potential for AF detection using smartphone-based PPG technology, but with insufficient evidence to demonstrate clinical utility at this time. Unrealistically high values for sensitivity and specificity were

found from predominantly small, single-centre studies (in meta-analysis, 94% and 97%, respectively). We identified high risk of bias, especially for the type of patients selected to take part, and insufficient information regarding study flow, design and timings. Additionally, there was evidence of publication bias with significant asymmetry indicating negative studies were less likely to be published (figure 4). In general, commercial smartphone applications were used for AF detection, but most studies lacked algorithm transparency. Information regarding data quality assessment and characterisation methods used to delineate AF from other arrhythmias (eg, atrial flutter, tachycardia or ectopics) was often missing, making replication and validation difficult. Taken together, these findings suggest the need for larger independent studies to assess the role of smartphone PPG for AF detection.

While AF is commonly associated with symptoms, asymptomatic episodes can occur and therefore only identified incidentally during routine medical review.³⁷ Patients with undiagnosed AF can present with an ischaemic stroke as their first clinical presentation, identified on an admission ECG or during subsequent monitoring.³⁸ There is a clear healthcare priority to increase effective screening in the community given the increasing prevalence of AF,¹ the substantial morbidity that is associated with undiagnosed AF, and the benefit of early detection and use of oral anticoagulation to prevent thromboembolism.⁷ The sporadic nature of AF illustrates a genuine need for non-invasive and scalable screening techniques that can be used to detect AF over a prolonged period of time. Current practice for AF screening consists mainly of opportunistic pulse palpation or detection using ECG and medical ambulatory devices, which have a limited monitoring duration.^{4,39} Hence, the development of new technology wherein patients can repeatedly monitor their own heart rhythm, providing more opportunity to pick up AF. With smartphones now a ubiquitous part of life in most communities across the world, the potential for widespread AF screening is now realisable. However, as with most new technologies, it is likely that hardware, software and algorithms will all need to develop to provide reliable information that can help direct clinical management.

This systematic review specifically addressed the value of PPG using smartphone technology, but other forms of PPG AF detection are also available. For example, the Apple Heart study used intermittent smartwatch-based PPG monitoring in 419 297 participants, of which 2161 (0.52%) received an irregular pulse alert. AF was newly detected in 153 or 450 (34%) participants who wore a 7-day ECG patch, giving a PPV for AF detection of 84%.^{37,40} The Huawei Heart study used smartwatches and smart

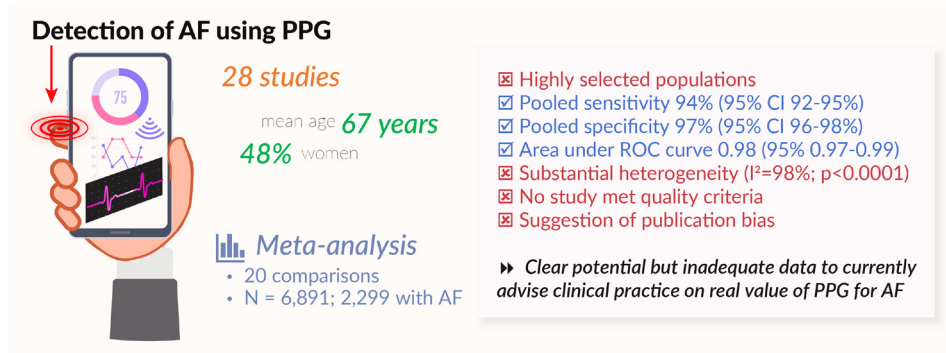


Figure 4 Graphical summary. A graphical summary of the main findings within this systematic review and meta-analysis. AF, atrial fibrillation; PPG, photoplethysmography.

bands in 187 912 participants, of which 424 (0.23%) received an irregular pulse notification and in those followed up, PPV was 92%.⁴¹ Both studies show the potential that PPG technology offers for accessible long-term self-monitoring, but also the limitations of requiring specific technology (in this case smart-watches) that often limits the population to younger individuals (only 6% were aged over 65 years in the Apple Heart study). This results in low AF detection rates, the potential for false positive cases, uncertain clinical impact (eg, in those without risk factors for thromboembolism) and hence high levels of unnecessary anxiety. There is also an issue of cost borne by the consumer, and exclusion of those with socioeconomic deprivation. Conversely, the number of smartphone users grows globally at an average of 11.8% annually, with increasing numbers across all age ranges, including those aged 65 and above (source: Statista), who have the most to gain from detecting AF.

This review highlights the need for real-world studies, with minimisation of selection bias to establish the true diagnostic accuracy of smartphone PPG. With a condition as heterogeneous as AF, it seems improbable that sensitivity and specificity values would be as high in an unselected population, meaning that false positives and false negatives would need careful consideration. With regard to smartphone applications, greater transparency from commercial providers regarding AF detection algorithms are required, and further work is needed to evaluate their role in the diagnostic pathway alongside conventional AF screening. Large-scale randomised clinical trials that are powered for endpoints such as stroke and cost-effectiveness are needed to compare these devices and establish their merits,³⁷ including studies that are independent of device or algorithm manufacturers.

Strengths and limitations

This systematic review is addressing a contemporary technology, with rapidly changing hardware and software. In order to capture the evolving field, we included data from published articles as well as conference abstracts, where findings may not have been peer reviewed or full information available. Ascertainment of study quality and bias was challenging for abstracts, and scores could improve following full-text publication. However, as many abstracts do not go on to a full-text publication, omitting these studies would have contributed to publication bias, particularly for studies with less positive or neutral results. The full range of study designs were included (retrospective, prospective and case-control studies), which may have led to an overestimation in diagnostic accuracy. Heterogeneity was substantial and there was evidence of possible publication bias. This is perhaps not surprising, as commercial companies that supported these studies may be less inclined to publish neutral studies or may have withheld developing results in order to protect their intellectual property. Due to the overall level of study quality, we were unable to separate results for low bias studies, and in particular selection bias is likely to have substantial impact on the generalisation of our findings.

CONCLUSION

Due to its paroxysmal nature in many patients, the detection of AF can be challenging using conventional ECG methods. With the growing use of smartphones, PPG technology offers the potential for large scale, non-invasive, patient-led screening of AF. PPG technology has shown promise for AF detection with high sensitivity and specificity. However, the current evidence base consists of small, biased and low-quality studies which are

insufficient to advise clinicians on the true value of PPG devices for AF detection. In view of the extensive global use of such devices, further research is urgently required with reference standards, standardised validation and transparent algorithms.

Key messages

What is already known on this subject?

- ⇒ With its rising prevalence and sporadic nature, early diagnosis of atrial fibrillation (AF) can prevent adverse events in at-risk patients.
- ⇒ Smartphone photoplethysmography (PPG) technology has the potential to offer widespread non-invasive community AF screening over a prolonged period of time.

What might this study add?

- ⇒ This systematic review and meta-analysis compared smartphone PPG applications with standard 1, 3 or 12-lead electrocardiograms for AF detection.
- ⇒ This meta-analysis showed unrealistically high sensitivity and specificity for AF detection, and identified concerns regarding study quality and bias, limiting applicability to current practice.

How might this impact on clinical practice?

- ⇒ This review demonstrates that at present there is insufficient evidence to recommend the use of smartphone PPG for AF detection in clinical practice.
- ⇒ Further independent large-scale studies are required to evaluate its role in diagnostic and screening purposes.

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Correction notice This article has been corrected since it was first published. The open access licence has been updated to CC BY.

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Contributors All authors are justifiably credited with authorship, according to the authorship criteria. In detail, SG, KVB, CS and DK are responsible for overall content, conception and design; SG and KVB for acquisition of data; SG, DK and VRC for analysis and interpretation of data; SG and DK for drafting the manuscript and final approval; SG, KVB, CS, VRC, NG, H-WU, JAW, K-SW, AB, FWA, MJCE, GG and DK for revision of manuscript and final approval. SG acted as guarantor.

Competing interests Dr Gill reports funding through the BigData@Heart Innovative Medicines Initiative, grant no.116074. Dr Bunting reports a grant from the University of Birmingham's British Heart Foundation Accelerator Award (BHF AA/18/2/34218). Dr Sartini reports that Bayer AG is one of the partners that have funded the IMI framework and is employed by Bayer AG in this IMI collaboration. Mr Roth Cardoso has nothing to disclose. Ms Narges Ghoreishi has nothing to disclose. Dr Uh reports grants and personal fees from Innovative Medicines Initiative 2 BigData@Heart, grant no. 116074, during the conduct of the study. Dr Williams has nothing to disclose. Dr Kiliana Suzart-Woischnik has nothing to disclose. Dr Banerjee reports grants from AstraZeneca, outside the submitted

work. Professor Asselbergs reports grants from Innovative Medicines Initiative 2 Joint Undertaking under grant agreement No (116074), during the conduct of the study and is supported by UCL Hospitals NIHR Biomedical Research Centre. Professor MJC Eijkemans has nothing to disclose. Professor Gkoutos has nothing to disclose. Professor Kotecha reports grants from the National Institute for Health Research (NIHR CDF-2015-08-074 RATE-AF; NIHR HTA-130280 DaRe2THINK; NIHR EME-132974 D2T-NV), the British Heart Foundation (PG/17/55/33087 and AA/18/2/34218), EU/EFPIA Innovative Medicines Initiative (BigData@Heart 116074), the European Society of Cardiology supported by educational grants from Boehringer Ingelheim/BMS-Pfizer Alliance/Bayer/Daiichi Sankyo/Boston Scientific, the NIHR/University of Oxford Biomedical Research Centre and British Heart Foundation/University of Birmingham Accelerator Award (STEER-AF NCT04396418), Amomed Pharma and IRCCS San Raffaele/Menarini (Beta-blockers in Heart Failure Collaborative Group NCT0083244); in addition to personal fees from Bayer (Advisory Board), AtriCure (Speaker fees), Protherics Medicines Development (Advisory Board) and Myokardia (Advisory Board).

Patient consent for publication Not applicable.

Provenance and peer review Not commissioned; externally peer reviewed.

Data availability statement Data sharing not applicable as no datasets generated and/or analysed for this study. This is a systematic review and meta-analysis of published and fully anonymised studies. The data used have already been published in journals in the form of full-text articles or conference abstracts.

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Smartphone detection of atrial fibrillation using photoplethysmography:

A systematic review and meta-analysis

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Supplementary material

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Table S1: Search strategy for EMBASE and MEDLINE databases

Search	Hits
('mobile application'/exp OR 'mobile app':ti,ab,de,tn,dn,kw OR 'mobile application':ti,ab,de,tn,dn,kw OR 'mobile applications':ti,ab,de,tn,dn,kw OR 'mobile apps':ti,ab,de,tn,dn,kw OR 'portable software app':ti,ab,de,tn,dn,kw OR 'portable software application':ti,ab,de,tn,dn,kw OR 'portable software applications':ti,ab,de,tn,dn,kw OR 'portable software apps':ti,ab,de,tn,dn,kw OR 'cell phone use'/exp OR 'cell phone usage':ti,ab,de,tn,dn,kw OR 'cell phone use':ti,ab,de,tn,dn,kw OR 'cell phone utilization':ti,ab,de,tn,dn,kw OR 'cellphone usage':ti,ab,de,tn,dn,kw OR 'cellphone use':ti,ab,de,tn,dn,kw OR 'cellphone utilization':ti,ab,de,tn,dn,kw OR 'mobile phone usage':ti,ab,de,tn,dn,kw OR 'mobile phone use':ti,ab,de,tn,dn,kw OR 'mobile phone utilization':ti,ab,de,tn,dn,kw OR 'mobile phone'/exp OR 'cell phone':ti,ab,de,tn,dn,kw OR 'cell phones':ti,ab,de,tn,dn,kw OR 'cellphone':ti,ab,de,tn,dn,kw OR 'cellphones':ti,ab,de,tn,dn,kw OR 'cellular phone':ti,ab,de,tn,dn,kw OR 'cellular telephone':ti,ab,de,tn,dn,kw OR 'mobile phone':ti,ab,de,tn,dn,kw OR 'mobile telephone':ti,ab,de,tn,dn,kw OR 'smartphone'/exp OR 'smart phone*':ti,ab,de,tn,dn,kw OR 'smartphone*':ti,ab,de,tn,dn,kw OR 'mobile app*':ti,ab,de,tn,dn,kw OR 'mobileapp*':ti,ab,de,tn,dn,kw OR 'portable software app*':ti,ab,de,tn,dn,kw OR 'portable software app*':ti,ab,de,tn,dn,kw OR ((mobile NEAR/2 app*):ti,ab,de,tn,dn,kw) OR (('cell phone* NEAR/2 app*):ti,ab,de,tn,dn,kw) OR (('cell phone* NEAR/2 software*):ti,ab,de,tn,dn,kw) OR (('cellphone* NEAR/2 app*):ti,ab,de,tn,dn,kw) OR (('cellphone* NEAR/2 software*):ti,ab,de,tn,dn,kw) OR (('cellular phone* NEAR/2 app*):ti,ab,de,tn,dn,kw) OR (('cellular phone* NEAR/2 software*):ti,ab,de,tn,dn,kw) OR (('cellularphone* NEAR/2 app*):ti,ab,de,tn,dn,kw) OR (('cellularphone* NEAR/2 software*):ti,ab,de,tn,dn,kw) OR (('cellular telephone* NEAR/2 app*):ti,ab,de,tn,dn,kw) OR (('cellular telephone* NEAR/2 software*):ti,ab,de,tn,dn,kw) OR (('cellulartelephone* NEAR/2 app*):ti,ab,de,tn,dn,kw) OR (('cellulartelephone* NEAR/2 software*):ti,ab,de,tn,dn,kw) OR ((mobile NEAR/2 (app* OR software*)):ti,ab,de,tn,dn,kw) OR 'cell phone*':ti,ab,tn,dn,de,kw OR 'cellphone*':ti,ab,tn,dn,de,kw OR 'cellular phone*':ti,ab,tn,dn,de,kw OR 'cellular telephone*':ti,ab,tn,dn,de,kw OR 'cellularphone*':ti,ab,tn,dn,de,kw OR 'cellulartelephone*':ti,ab,tn,dn,de,kw OR 'mobile phone*':ti,ab,tn,dn,de,kw OR 'mobile telephone*':ti,ab,tn,dn,de,kw OR 'smart phone*':ti,ab,tn,dn,de,kw OR 'smartphone*':ti,ab,tn,dn,de,kw) AND ('tachycardia'/exp OR 'catecholaminergic polymorphic ventricular tachycardia'/exp OR 'experimental tachycardia'/exp OR 'isoprenaline-induced tachycardia'/exp OR 'heart ventricle tachycardia'/exp OR 'hyperkinetic heart syndrome'/exp OR 'monomorphic ventricular tachycardia'/exp OR 'pacemaker mediated tachycardia'/exp OR 'paroxysmal tachycardia'/exp OR 'paroxysmal supraventricular tachycardia'/exp OR 'wolff parkinson white syndrome'/exp OR 'polymorphic ventricular tachycardia'/exp OR 'postural orthostatic tachycardia syndrome'/exp OR 'reentry tachycardia'/exp OR 'atrioventricular nodal reentry tachycardia'/exp OR 'sinoatrial nodal reentry tachycardia'/exp OR 'sinus tachycardia'/exp OR 'supraventricular tachycardia'/exp OR 'ectopic atrial tachycardia'/exp OR 'junctional ectopic tachycardia'/exp OR 'tachycardia induced cardiomyopathy'/exp OR 'acute atrial fibrillation':ti,ab,tn,dn,kw,de OR 'acute heart atrium fibrillation':ti,ab,tn,dn,kw,de OR 'atrial fibrillation':ti,ab,tn,dn,kw,de OR 'atrium fibrillation':ti,ab,tn,dn,kw,de OR 'auricular fibrillation':ti,ab,tn,dn,kw,de OR 'auricular fibrillation':ti,ab,tn,dn,kw,de OR 'cardiac atrial fibrillation':ti,ab,tn,dn,kw,de OR 'cardiac atrium fibrillation':ti,ab,tn,dn,kw,de OR 'chronic atrial fibrillation':ti,ab,tn,dn,kw,de OR 'chronic atrium fibrillation':ti,ab,tn,dn,kw,de OR 'experimental atrial fibrillation':ti,ab,tn,dn,kw,de OR 'experimentally induced atrial fibrillation':ti,ab,tn,dn,kw,de OR 'fibrillation, heart atrium':ti,ab,tn,dn,kw,de OR 'heart atrial fibrillation':ti,ab,tn,dn,kw,de OR 'heart atrium fibrillation':ti,ab,tn,dn,kw,de OR 'heart fibrillation atrium':ti,ab,tn,dn,kw,de OR 'new-onset atrial fibrillation':ti,ab,tn,dn,kw,de OR 'nonvalvular atrial fibrillation':ti,ab,tn,dn,kw,de OR 'non-valvular atrial fibrillation':ti,ab,tn,dn,kw,de OR 'paroxysmal atrial fibrillation':ti,ab,tn,dn,kw,de OR 'paroxysmal heart atrium fibrillation':ti,ab,tn,dn,kw,de OR 'permanent atrial fibrillation':ti,ab,tn,dn,kw,de OR 'permanent atrium fibrillation':ti,ab,tn,dn,kw,de OR 'persistent atrial fibrillation':ti,ab,tn,dn,kw,de OR 'persistent atrium fibrillation':ti,ab,tn,dn,kw,de OR 'persistent heart atrium fibrillation':ti,ab,tn,dn,kw,de OR 'recent-onset atrial fibrillation':ti,ab,tn,dn,kw,de OR 'atrial fibrillation'/exp OR 'chronic atrial fibrillation'/exp OR 'experimental atrial fibrillation'/exp OR 'new-onset atrial fibrillation'/exp OR 'paroxysmal atrial fibrillation'/exp OR 'permanent atrial fibrillation'/exp OR 'persistent atrial fibrillation'/exp OR (((atrial* OR atrium* OR auricular*) NEXT/2 fibrillat*):ti,ab,tn,dn,kw,de) OR 'heart atrium flutter'/exp OR 'atrial flutter':ti,ab,tn,dn,kw,de OR 'atrium flutter':ti,ab,tn,dn,kw,de OR 'atrium flutter, heart':ti,ab,tn,dn,kw,de OR 'auricular flutter':ti,ab,tn,dn,kw,de OR 'cardiac atrial flutter':ti,ab,tn,dn,kw,de OR 'cardiac atrium flutter':ti,ab,tn,dn,kw,de OR 'flutter, heart atrium':ti,ab,tn,dn,kw,de OR 'heart atrial flutter':ti,ab,tn,dn,kw,de OR 'heart atrium flutter':ti,ab,tn,dn,kw,de OR 'supraventricular flutter':ti,ab,tn,dn,kw,de OR (((atrial* OR auricular*) NEXT/2 flutter*):ti,ab,tn,dn,kw,de) OR 'heart ventricle flutter'/exp OR 'flutter, heart ventricle':ti,ab,tn,dn,kw,de OR 'heart ventricle flutter':ti,ab,tn,dn,kw,de OR 'ventricular flutter':ti,ab,tn,dn,kw,de OR ((ventri* NEXT/2 flutter*):ti,ab,tn,dn,kw,de) OR 'heart ventricle fibrillation'/exp OR 'cardiac ventricle fibrillation':ti,ab,tn,dn,kw,de OR 'cardiac ventricular fibrillation':ti,ab,tn,dn,kw,de OR 'fibrillation, heart ventricle':ti,ab,tn,dn,kw,de OR 'heart ventricle fibrillation':ti,ab,tn,dn,kw,de OR 'heart ventricular	781

<p>fibrillation':ti,ab,tn,dn,kw,de OR 'ventricle fibrillation':ti,ab,tn,dn,kw,de OR 'ventricle fibrillation, heart':ti,ab,tn,dn,kw,de OR 'ventricular fibrillation':ti,ab,tn,dn,kw,de OR 'experimental ventricular fibrillation'/exp OR 'experimental ventricular fibrillation':ti,ab,tn,dn,kw,de OR 'experimentally induced ventricular fibrillation':ti,ab,tn,dn,kw,de OR 'electrically induced ventricular fibrillation'/exp OR 'electrically induced ventricular fibrillation':ti,ab,tn,dn,kw,de OR ((ventri* NEXT/2 fibrill*):ti,ab,tn,dn,kw,de) OR 'heart beat'/exp OR 'beat, heart':ti,ab,tn,dn,kw,de OR 'cardiac beat':ti,ab,tn,dn,kw,de OR 'heart beat':ti,ab,tn,dn,kw,de OR 'diastole'/exp OR 'cardiac diastole':ti,ab,tn,dn,kw,de OR 'diastole':ti,ab,tn,dn,kw,de OR 'diastolic force':ti,ab,tn,dn,kw,de OR 'heart diastole':ti,ab,tn,dn,kw,de OR 'extrasystole'/exp OR 'beat, ectopic':ti,ab,tn,dn,kw,de OR 'cardiac complexes, premature':ti,ab,tn,dn,kw,de OR 'ectopic beat':ti,ab,tn,dn,kw,de OR 'extrasystole':ti,ab,tn,dn,kw,de OR 'extrasystolic beat':ti,ab,tn,dn,kw,de OR 'heart extrasystole':ti,ab,tn,dn,kw,de OR 'heart premature beat':ti,ab,tn,dn,kw,de OR 'nodal extrasystole':ti,ab,tn,dn,kw,de OR 'premature beat':ti,ab,tn,dn,kw,de OR 'systole'/exp OR 'heart systole':ti,ab,tn,dn,kw,de OR 'systole':ti,ab,tn,dn,kw,de OR 'systolic index':ti,ab,tn,dn,kw,de OR 'systolic phase':ti,ab,tn,dn,kw,de OR ((heart NEXT/3 beat):ti,ab,tn,dn,kw,de) OR ((irregular* NEAR/3 (puls* OR heart* OR rhythm*)):ti,ab,tn,dn,kw,de) OR (((atypical* OR unexpect* OR unsuspect* OR unforeseeabl* OR abnormal* OR uneven* OR fitful* OR erratic* OR sporadi*) NEAR/3 (puls* OR heart* OR rhythm*)):ti,ab,de,tn,dn,kw))</p>	
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Table S2: Search strategy for Cochrane database

ID	Search	Hits
#1	MeSH descriptor: [Atrial Fibrillation] explode all trees	4665
#2	(atrial* near/2 fibrillation*):ti,ab,kw	12671
#3	#1 OR #2	12671
#4	MeSH descriptor: [Atrial Flutter] explode all trees	375
#5	(atrial* near/2 flutter*):ti,ab,kw	978
#6	#4 OR #5	978
#7	MeSH descriptor: [Ventricular Fibrillation] explode all trees	544
#8	(ventri* near/2 fibrillat*):ti,ab,kw	1713
#9	#7 OR #8	1713
#10	MeSH descriptor: [Tachycardia] explode all trees	1799
#11	tachycardi*:ti,ab,kw	8496
#12	#10 OR #11	8525
#13	MeSH descriptor: [Heart Rate] explode all trees	19310
#14	(heart rate):ti,ab,kw	75355
#15	#13 OR #14	75360
#16	(Irregular* or unpredictable* or atypical*) near/3 (puls* or heart* or rhythm*)	244
#17	(atypical* or unexpect* or unsuspect* or unforeseeabl* or abnormal* or uneven* or fitful* or erratic* or sporadi*) near/3 (puls* or heart* or rhythm*)	946
#18	#16 OR #17	1157
#19	((smart* near/2 phone*) or (mobil* near/2 phone*) or mobilphone* or cellphone* or (cell near/2 phone*) or mobilephone or mobile app*):ti,ab,kw	8221
#20	MeSH descriptor: [Mobile Applications] explode all trees	660
#21	MeSH descriptor: [Smartphone] explode all trees	407
#22	MeSH descriptor: [Cell Phone] explode all trees	1373
#23	#19 OR #20 OR #21 OR #22	8851
#24	MeSH descriptor: [Ventricular Flutter] explode all trees	2
#25	(ventri* near/2 flutter*):ti,ab,kw	28
#26	#24 OR #25	28
#27	#3 OR #6 OR #9 OR #12 OR #15 OR #18 OR #26	90651
#28	#23 AND #27 in Trials	370

Table S3: Summary of characteristics for conference abstracts

Study	Study design and key enrolment criteria	Setting and sample size	Population characteristics	Technology for AF detection	Reference test
Grieten 2018-1 ¹	Prospective multi-centre Age>65 years	Primary care N=242 AF prevalence 38%	Age 77 years (mean); Female 57%; hypertension 84%; diabetes 22%; stroke 23%; heart failure 29%; OAC 55%	Unspecified smartphone; Fibrichck PPG app and algorithm	Single lead ECG
Grieten 2018-2 ²	Prospective, multi-centre	Primary care N=1056 AF prevalence 0.8%	Age 59 years (mean); Female 59%	Unspecified smartphone; Fibrichck PPG app and algorithm	Single lead ECG
Karim 2017 ³	Prospective, single centre Sinus arrhythmia and ectopics excluded	Secondary care N=140 AF prevalence 50%		Unspecified smartphone; PPG Preventicus app and algorithm	12-lead ECG
Kuan 2018 ⁴	Prospective, single centre	Secondary care N=194 AF prevalence 35%	Age 70 years (mean); Female 27%	iPhone; CRMA app 3 X 20 second recordings, AF labelled if pulse irregularity found in ≥ 1 PPG readings or 3 uninterpretable readings	12 lead ECG
Maitas 2012-1 ⁵	Prospective, single centre AF for DCCV	Secondary care N=52 AF prevalence 100%		iPhone 4S; unknown PPG app, 120 second recordings, analysed using 2 statistical techniques (RMSSD, Shannon entropy) to examine heart beat intervals and beat-to-beat variability	12-lead ECG
Maitas 2012-2 ⁶	Prospective, single centre AF for DCCV	Secondary care N=33 AF prevalence 100%		iPhone 4S; unknown PPG app, 120-300 second recordings, analysed using 3 statistical techniques (RMSSD, ShE and Sample entropy)	12-lead ECG

Mortelmans 2017 ⁷	Prospective, single centre Majority with history of AF	Primary care N=242 AF prevalence 66%		Unspecified smartphone; Fibrichck PPG app, 60 second recording	Single lead ECG
Mutke 2019 ⁸	Retrospective analysis of data from 2 prospective multi-centre validation trials	Unclear N=1096 AF prevalence 44%		Unspecified smartphone and PPG app; 60 second recording automated signal quality check and categorized into AF or SR using unspecified algorithm	Blinded interpretation of single lead ECG by cardiologists
Napolitano 2015 ⁹	Retrospective analysis of pulse recordings from patients who underwent DCCV	Data form secondary care N=121 AF prevalence 81%		iPhone 4S; PULSES MART app, 120 second recording analysed using 3 statistical techniques RMSSD; ShE; Poincare plot	12 or 3 lead ECG
Proesmans 2019-2 ¹⁰	Prospective, single centre AF for DCCV and in-patients with AF	Secondary care N=164 AF prevalence 37%	Age 64 years (mean); Females 42%	7 iOS and 7 android smartphones; unknown PPG app	12 lead ECG
Proesmans. 2018 ¹¹	Prospective, 2 centre Age over 40 years	Primary care N=1095 AF prevalence 0.5%		Unknown smartphone and PPG app; automatic algorithm and visual interpretation	Single lead ECG
Rozen 2017 ¹²	Prospective, single centre AF undergoing DCCV	Secondary care N=113 AF prevalence 100%	68 years (mean); Female 23%	iPhone; CRMA PPG app, 6 recordings analysed by algorithm 2 out of 3 irregular recordings needed to label AF	Blinded 12 lead ECG or single lead ECG (rhythm strip) interpretation by 2 cardiologists
Siu 2016 ¹³	Prospective, single centre Either >65 years, DM, or hypertension	Primary care N= 1027 AF prevalence 3%	Age 68 years (mean)	Unspecified smartphone; CRMA PPG app	Single lead ECG interpretation by 2 cardiologists

Smeets 2019 ¹⁴	Prospective single centre AF scheduled for DCCV/ablation & those on continuous monitoring	Secondary care N=150 AF prevalence 37%	64 years (mean); Females 42% (AF)	6 Android and 2 iOS smartphones; unknown PPG app; 1 recording per device	12-lead ECG
Vaid 2015 ¹⁵	Prospective single centre AF undergoing DCCV	Secondary care N= 37 AF prevalence 78%	69 years (median); Female 19%	iPhone; CRMA PPG, 6 recordings analysed by CRMA algorithm 2 out of 3 irregular recordings needed to label AF	Blinded 12 lead ECG or single lead ECG (rhythm strip) interpretation by 2 cardiologists
Vandenberk 2018-1 ¹⁶	Prospective single centre History of AF	Unclear N=344 AF prevalence 50%		Unspecified smartphone, Fibrichck PPG app, analysed by 2 blinded cardiologists	Blinded 12 lead ECG analysis by 2 cardiologists
Vandenberk 2018-2 ¹⁷	Prospective single centre History of AF	Unclear N= 322 AF prevalence 55%		Unspecified smartphone and PPG app, 60 second recording analysed by clinicians	Blinded single lead ECG interpretation by 2 cardiologists
Yan 2016 ¹⁸	Prospective single centre	Secondary N=85 AF prevalence 29%	Age 72 years (mean); Female 33%	iPhone 6s, CRMA PPG app, 3 X 20 second recordings, irregularity in 1 or more recordings needed to label AF	12 lead ECG

Table S4: Risk of bias and applicability concerns for full text studies

Study author and year	QUADAS 2-Risk of Bias				QUADAS 2-Applicability concerns			
	Patient selection	Index test: PPG	Reference standard: ECG	Flow and timing	Patient Selection	Index test: PPG	Reference standard: ECG	Domains with high risk
Brasier 2019 ¹⁹	High risk	Unclear	Low risk	High risk	Low risk	Low risk	Low risk	2/7
Chan 2016 ²⁰	Unclear	Low risk	Low risk	High risk	Low risk	Low risk	Low risk	1/7
Fan 2019 ²¹	High risk	Unclear	Low risk	High risk	Low risk	Low risk	Low risk	2/7
McManus 2016 ²²	High risk	Low risk	Unclear	High risk	Low risk	Low risk	Low risk	2/7
McManus 2013 ²³	High risk	High risk	Unclear	Low risk	Low risk	Low risk	Low risk	2/7
Mutke 2020 ²⁴	High risk	Low risk	Low risk	High risk	Low risk	Low risk	Low risk	2/7
Poh 2018 ²⁵	Unclear	Low risk	High risk	High risk	Unclear	Low risk	Low risk	2/7
Proesmans 2019-1 ²⁶	High risk	Unclear	Low risk	High risk	Low risk	Low risk	Low risk	2/7
Rozen 2018 ²⁷	High risk	Low risk	Low risk	High risk	Low risk	Low risk	Low risk	2/7
Yan 2018 ²⁸	High risk	Low risk	Low risk	High risk	Low risk	Low risk	Low risk	2/7

Table S5: Risk of bias and applicability concerns for conference abstracts

Study author and year	QUADAS 2-Risk of Bias				QUADAS 2-Applicability concerns			
	Patient selection	Index test: PPG	Reference standard: ECG	Flow and timing	Patient Selection	Index test: PPG	Reference standard: ECG	Domains with high risk
Grieten 2018-1 ¹	High risk	Unclear	Low risk	High risk	Low risk	Low risk	Low risk	2/7
Grieten 2018-2 ²	High risk	Unclear	High risk	High risk	Low risk	Low risk	Low risk	3/7
Karim 2017 ³	High risk	Unclear	Unclear	Unclear	Low risk	Low risk	Low risk	1/7
Kuan 2018 ⁴	Unclear	Unclear	Unclear	Unclear	Unclear	Low risk	Low risk	0/7
Maitas 2012-1 ⁵	High risk	Unclear	Unclear	Unclear	Low risk	Low risk	Low risk	1/7
Maitas 2012-2 ⁶	High risk	Unclear	Unclear	Unclear	Low risk	Low risk	Low risk	1/7
Mortelmans 2017 ⁷	High risk	Unclear	High risk	High risk	Low risk	Low risk	Low risk	3/7
Mutke 2019 ⁸	Unclear	Unclear	Low risk	Low risk	Low risk	Low risk	Low risk	0/7
Napolitano 2015 ⁹	High risk	Unclear	Unclear	High risk	Low risk	Low risk	Low risk	2/7
Proesmans 2019-2 ¹⁰	Unclear	Unclear	High risk	Unclear	Unclear	Low risk	Low risk	1/7
Proesmans 2018 ¹¹	High risk	Unclear	Unclear	High risk	Low risk	Low risk	Low risk	2/7
Rozen 2017 ¹²	High risk	Low risk	Low risk	High risk	Low risk	Low risk	Low risk	2/7
Siu 2016 ¹³	Unclear	Unclear	Unclear	Unclear	Low risk	Low risk	Low risk	0/7
Smeets. 2019 ¹⁴	Unclear	Unclear	Unclear	High risk	Low risk	Low risk	Low risk	1/7
Vaid 2015 ¹⁵	High risk	Low risk	Low risk	High risk	Low risk	Low risk	Low risk	2/7
Vandenberk 2018-1 ¹⁶	High risk	Unclear	Unclear	Unclear	Low risk	Low risk	Low risk	1/7
Vandenberk 2018-2 ¹⁷	Unclear	Unclear	Low risk	Unclear	Low risk	Low risk	Low risk	0/7
Yan 2016 ¹⁸	Unclear	Low risk	Unclear	Unclear	Low risk	Low risk	Low risk	0/7

Table S6: Sensitivity and specificity of each study by smartphone PPG application

Application	Study	Sensitivity % (95% CI)	Specificity (95% CI)
Cardiio Rhythm	Chan 2016 ²⁰	93 (77-99)	98 (97-99)
	Rozen 2018 ²⁷	93 (87-97)	91 (83– 96)
	Yan 2018a ²⁸	95 (87-98)	96 (91-98)
	Yan 2018b ²⁸	95 (87-98)	93 (88-96)
	Kuan 2018 ⁴	100 (83-100)	95 (84-99)
	Rozen 2017 ¹²	96 (90-99)	93 (87-97)
	Siu 2016 ¹³	93	98
	Vaid 2015 ¹⁵	97 (82-100)	85 (69-94)
	Yan 2016 ¹⁸	93 (77-98)	95 (86-98)
Preventicus	Brasier 2019a ¹⁹	90 (86-93)	99 (98-100)
	Brasier 2019b ¹⁹	91 (87-95)	99 (97-100)
	Brasier 2019c ¹⁹	92 (86-95)	100 (98-100)
	Fan 2019 ²¹	95 (92-97)	100 (98-100)
	Karim 2017 ³	94 (85-98)	96 (87-99)
	Mutke 2020 ²⁴	92 (89-94)	98 (97-99)
Fibricheck	Proesmans 2019-1 ²⁶	96 (89-99)	97 (91-99)
	Grieten 2018-1 ¹	98 (92-100)	88 (80-94)
	Grieten 2018-2 ²	100	97
	Mortelmans 2017 ⁷	98 (92-100)	88 (80-94)
	Vandenberk 2018-1 ¹⁶	97	99
PULSE-SMART	McManus 2016 ²²	97	94
	Napolitano 2015 ⁹	97	94

Figure S1: Forest plot of the sensitivity and specificity of smartphone PPG vs ECG

Horizontal lines represent the 95% confidence interval (where available) for each comparison.

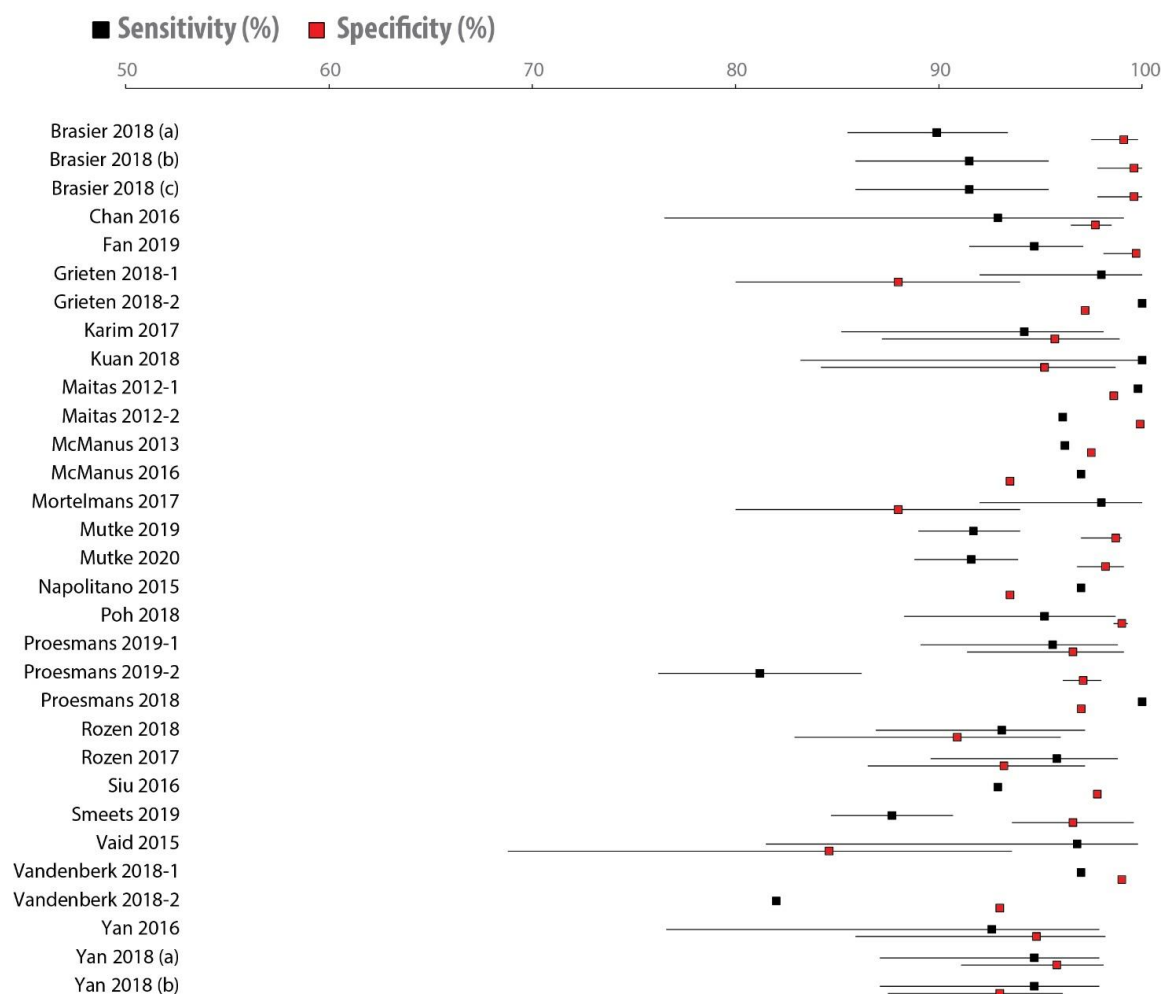
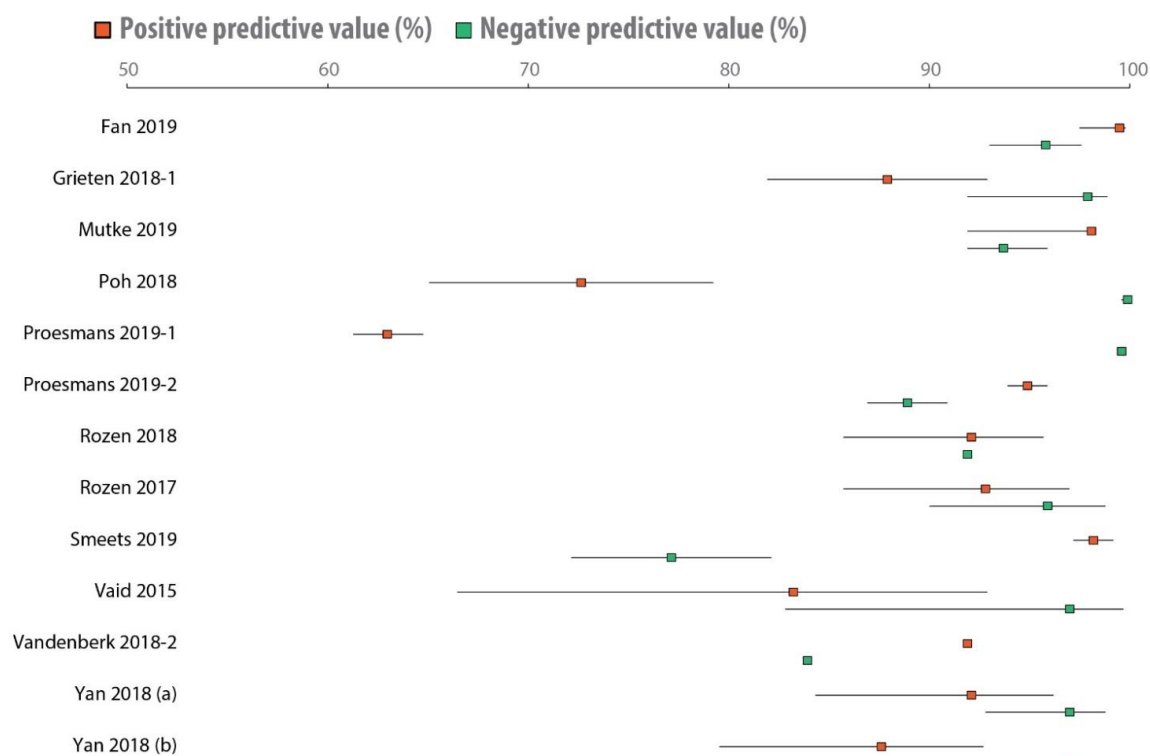


Figure S2: Forest plot of positive/negative prediction for smartphone PPG vs ECG

Horizontal lines represent the 95% confidence interval (where available) for each comparison



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