A METHOD OF TESTING IMPLANTED CARDIAC PACEMAKERS

BY

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Received October 14, 1964

In some patients with complete heart block electrical pacing has become an accepted form of treatment, and this has been well reviewed (Chardack, Gage, and Greatbatch, 1960; Chardack 1964; Zoll et al., 1961; Portal et al., 1962). The quoted battery life of pacemakers available commercially is from 2 to 5 years. However, experience with our first 10 cases has shown that earlier replacement of the units is sometimes necessary because of premature battery failure and either gradual or sudden failure of another component. These failures cause changes in one or more of the following output characteristics of the pacemaker: rate, amplitude, and pulse width. Measurement of these characteristics is easily made with the pacemaker outside the body, but after the unit is implanted this presents some difficulty. Pulse rate of the unit can be obtained from the electrocardiogram, but output voltage and pulse width are more difficult to measure. One commercial model* provides two subcutaneous testing electrodes to which needles can be attached under local anaesthetic, but it is possible for these wires to break while the unit is functioning correctly (Parsonnet et al., 1963).

The standard electrocardiogram from a patient with an implanted pacemaker shows the stimulating pulses (Fig. 1), but their wave form is not accurately reproduced because of the limited frequency response of the recorder. However, if the electrocardiogram is viewed on a calibrated cathode ray oscilloscope with an adequate frequency response, and with the time-base sweep triggered from each pulse, measurement can be made on the amplitude and width of these pulses in any particular lead (Fig. 2). The wave form of the pulse is a replica of the current output wave form of the pacemaker. Our studies with animals have confirmed that the amplitude in a particular lead is directly proportional to the amplitude of the stimulating pulse (Fig. 3). The amplitude was found to be in the range 0–350 mV depending on the angle between the dipole of the stimulating electrodes and the electrocardiogram lead. The amplitude varied up to 20 mV with respiration, and also varied up to 25 per cent depending on posture.

SUBJECTS AND METHOD

Ten patients with implanted pacemakers have been studied at intervals of from 2 to 8 weeks after insertion of the units (Table I). With the patient lying in the standard electrocardiographic position, german silver electrodes were attached to the limbs after careful preparation. The right leg was earthed, and the other electrodes (Fig. 4) were connected via a lead selector to a calibrated differential input oscilloscope†.

* Medtronic pacemaker—Models 5870 and 5860.
† Tektronix types 502 and 564.
I. Introduction

Fig. 1—Electrocardiographic leads I, II, and III from a patient with an implanted pacemaker using unipolar stimulation. The arrows show the small pulse preceding each ventricular complex. The pulses in leads II and III are more than 100 mV amplitude but are not accurately reproduced because of the limited frequency response of the recorder.

Fig. 2.—Photograph from the screen of a cathode ray oscilloscope showing the pulse from unipolar pacing electrodes seen in lead III of the electrocardiogram. The horizontal speed has been increased to 0.5 millisecond per division, and the vertical scale is 50 mV per division.

Fig. 3.—Relationship between the amplitude of the pulse from the stimulating electrodes seen in lead III and the actual stimulating potential in an anaesthetized dog with a unipolar stimulating electrode system. Maximum and minimum points show the amplitude variation with respiration.

Fig. 4.—Electrocardiograph electrodes and lead selector connected to a differential input cathode ray oscilloscope. The horizontal sweep was set to trigger from the pacemaker pulses, and the amplitude and pulse width were measured from leads I, II, and III in turn.
### Table

##### Data Relating to Pacemakers in Ten Patients

<table>
<thead>
<tr>
<th>Case No.</th>
<th>Indication</th>
<th>Date of Implant</th>
<th>Type of Pacemaker</th>
<th>Longevity of Unit (mth.)</th>
<th>Outcome</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>May 1961</td>
<td>Elema 137 bipolar electrodes</td>
<td>—</td>
<td>Sudden death probably due to ventricular fibrillation 2 mth. after implant</td>
</tr>
<tr>
<td>2</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>April 1962</td>
<td>Elema 137 bipolar electrodes</td>
<td>12</td>
<td>Unit removed because of battery failure</td>
</tr>
<tr>
<td></td>
<td></td>
<td>April 1963</td>
<td>Elema 137 bipolar electrodes</td>
<td>12</td>
<td>Unit removed because of 14% rise in rate and 45% decrease in pulse-width</td>
</tr>
<tr>
<td>3</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>March 1963</td>
<td>Elema 137 bipolar electrodes</td>
<td>6</td>
<td>Unit still operating satisfactorily after 4 mth.</td>
</tr>
<tr>
<td>4</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>July 1963</td>
<td>Elema 137 bipolar electrodes</td>
<td>4½</td>
<td>Unit removed because of 23% rise in rate</td>
</tr>
<tr>
<td>5</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>March 1963</td>
<td>St. George's unipolar electrodes</td>
<td>—</td>
<td>Unit exteriorized after 3½ mth. because of infection; pacing continued through same wires</td>
</tr>
<tr>
<td>6</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>May 1963</td>
<td>St. George's unipolar electrodes</td>
<td>9</td>
<td>Death 2 wk. after implant due to pacing failure associated with purulent pericarditis</td>
</tr>
<tr>
<td></td>
<td></td>
<td>March 1964</td>
<td>St. George's unipolar electrodes</td>
<td>—</td>
<td>Death 2 days post-operatively; pacing failure due to unknown cause</td>
</tr>
<tr>
<td>7</td>
<td>Complete heart-block; heart failure</td>
<td>July 1963</td>
<td>St. George's unipolar electrodes</td>
<td>—</td>
<td>Unit still operating satisfactorily</td>
</tr>
<tr>
<td>8</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>July 1963</td>
<td>St. George's unipolar electrodes</td>
<td>—</td>
<td>Unit still operating satisfactorily</td>
</tr>
<tr>
<td>9</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>Dec. 1963</td>
<td>St. George's unipolar electrodes</td>
<td>—</td>
<td>Unit still operating satisfactorily</td>
</tr>
<tr>
<td>10</td>
<td>Complete heart-block; Stokes-Adams attacks</td>
<td>June 1964</td>
<td>St. George's unipolar electrodes</td>
<td>—</td>
<td>Unit still operating satisfactorily</td>
</tr>
</tbody>
</table>
The horizontal sweep was set to trigger from the pacemaker pulse and the amplitude and pulse-width were recorded from leads I, II, and III. The amplitude was measured during normal breathing, held inspiration and held expiration, and the rate was measured. All tests on one patient over a period of 10 months are shown in Fig. 5. Fig. 6 shows a more convenient method of displaying the progressive results.

Before each test the horizontal calibration of the cathode ray oscilloscope was checked by using a crystal-controlled Time-mark generator, and the vertical scale was checked against a standard voltage cell.

**RESULTS**

The results of tests on four patients are reported to demonstrate typical findings from units with unipolar and bipolar stimulating electrodes.

**CASE REPORTS**

**Case 2.** A 64-year-old woman with complete heart block had recurrent Stokes-Adams attacks which could only be controlled by a right ventricular electrode catheter. An Elema pacemaker (type 137) was implanted using a bipolar electrode system. No tests were done on this unit. Because of premature battery failure it was replaced after 12 months with a second Elema unit which was tested 4 days after implant and then at intervals of 4 to 14 weeks. As seen in Fig. 7, the rate fell considerably for about 5 months and then increased progressively. Over the first 4 months the pulse width remained constant but then decreased progressively. The pulse amplitude in all leads was in the range 0–60 mV and no over-all change was detected. Because of the continual decrease in pulse width and increase in pulse rate, the unit was removed 12 months after implant. On examination the pulse width was found to have fallen to the value indicated before removal. A new pacemaker inserted at that time has remained stable.

**Case 6.** A 68-year-old diabetic woman had complete heart block and Stokes-Adams attacks which failed to respond to medical treatment. A St. George's pacemaker with unipolar electrodes was implanted

* Tektronix type 180-A Time-mark generator.
in June 1963. The unit was tested soon after implant and then at intervals of from 4 to 8 weeks (see Fig. 6). The pulse amplitude in all leads fell considerably over the first 8 weeks, remained relatively constant until 24 weeks, and then fell suddenly to 60 per cent by 37 weeks. The rate began to increase 16 weeks after implant and by 37 weeks had reached 115 a minute. The pulse width began to decrease 20 weeks after implant and by 37 weeks had decreased by 25 per cent. The unit was removed 37 weeks after implant and tested. The output voltage amplitude was found to have fallen to 60 per cent of the original value and the pulse width had decreased by 25 per cent.

Case 7. A 67-year-old man with complete heart block and recurrent syncopal attacks was treated in August 1963, by insertion of a St. George's pacemaker with unipolar electrodes. The rate decreased over the first 3 months, returned to approximately the original value in the next 3 months, and then decreased again (see Fig. 8). The pulse width increased steadily after implant. The pulse amplitude decreased over the first 3 months and then remained relatively constant, and the unit is continuing to operate satisfactorily.

Case 8. A 64-year-old man was treated for complete heart block by implanting a St. George's pacemaker with unipolar electrodes. The pulse rate was relatively constant over the first three months but then increased slightly (Fig. 9). The pulse amplitude in leads II and III increased over the first 2 weeks, returned to its original value over the next 2 weeks, and has remained relatively constant for 12 months. The unit is continuing to operate satisfactorily.

**DISCUSSION**

Measurement of the pacemaker pulse in any electrocardiographic lead, in a patient with either unipolar or bipolar stimulating electrodes, will show the width of the stimulating pulse. Any change in pulse width is an indication of change in pacemaker operation and must be regarded as significant. Large changes in pulse width are important because of the danger of loss of stimulation below about 0·5 millisecond and the risk of ventricular fibrillation with long pulses (Race,
Stirling, and Emery, 1963). Case 2 demonstrates the situation where the pulse width from a unit continually narrowed, while the rate increased (Fig. 7). These two variations strongly suggested failure of a component affecting both the width and rate of the output pulses. The unit was removed and on investigation the pulse width measurement was found to have been correct.

It is important to know if any change has occurred in the amplitude of the stimulating pulse, especially in the case of the pacemaker losing control of ventricular action. Though our experience has shown that the amplitude of the pulse in any lead is directly proportional to the amplitude of the stimulating potential, it changes by about 10–15 per cent from week to week with constant stimulating potential. This is most pronounced in the first 8 weeks following implant and is seen best in Cases 6, 7, and 8. When the batteries are new and the output from the pacemaker can be assumed constant, these initial variations are due to changes in the tissues around the electrodes following suturing. This would cause changes in the electrical field in the patient. The long-term variations in pulse amplitude are poorly understood but are probably due to physical changes in the patient. We took the over-all trend of pulse amplitude, not fluctuations, as an indication of change in stimulating potential.

In the patients with unipolar stimulation (Cases 6, 7, and 8) a long vertical dipole was formed in the body by the electrodes, the negative electrode on a ventricle and the indifferent electrode under the rectus abdominus muscle. Large voltages (100–300 mV) were produced in the vertical leads II and III, and small voltages between the arms in lead I. Patients with bipolar electrode systems had pulse amplitudes in the range 0–60 mV in all leads because of the short dipole formed on the heart by the two ventricular electrodes.

In Case 6 the amplitude in leads II and III decreased to 60 per cent from a relatively steady value over the five months from August 1963 to January 1964. On removal of the unit the output
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voltage was found to have fallen to 60 per cent of the original value. Thus we were able to confirm that a relatively large decrease in amplitude in leads II and III together, with a unipolar electrode system, is reliable evidence of a drop in output voltage amplitude.

In Case 2 (a patient with bipolar electrodes), the pulse amplitude was, at the most, twice as large as the deviation due to respiration and week-by-week changes. Thus the small pulses from a bipolar system do not give a good indication of stimulating potential.

Since both systems of electrode placement will give satisfactory stimulation, we now consider it preferable to use a unipolar system with the indifferent electrode well away from the heart, because this system gives reliable indication of changes in stimulating pulse amplitude. These measurements, with that of pulse rate, give good criteria for assessing the condition of implanted pacemakers. If the circuit of the unit is known it should be possible to diagnose individual faulty components.

**SUMMARY**

Ten patients with implanted pacemakers have been studied at regular intervals, and 4 are reported.

A simple procedure for testing implanted pacemakers has been developed. It consists of measuring the stimulating pulses in the standard electrocardiographic leads when displayed on a cathode ray oscilloscope.

Though the method can be used with unipolar or bipolar electrode systems, more information can be obtained from a unipolar system.

We wish to thank Mr. I. H. McConchie, Mr. J. I. Hayward, and Mr. L. Grigg for implanting the pacemakers and for their interest and support of the project.

**REFERENCES**