

REVIEW

Cardiac output in 1998

M Singer

Over 100 years ago Karl Ludwig stated that:

The fundamental problems in the circulation derive from the fact that the supply of adequate amounts of blood to the organs of the body is the main purpose of the circulation while the pressures that are necessary to achieve it are of secondary importance; but the measurement of flow is difficult while that of pressure is easy so that our knowledge of flow is usually derivatory.

Are we, in 1998, any nearer to the routine monitoring of flow? The more salient question may be whether flow measurement is actually useful in terms of clinical management or patient outcome. The wherewithal to monitor flow exists. Techniques for cardiac output measurement, albeit of varying accuracy, invasiveness and complexity, have been available commercially for the past 25 years, although their use in the UK is relatively sparse, both in intensive and coronary care units¹ and operating theatres.² The national confidential enquiry into perioperative deaths² covering the years 1993–94 reviewed 1802 deaths occurring within 30 days of an operation. Three quarters of these patients were deemed moderate to very high risk, yet only 4.2% had a Swan-Ganz (pulmonary artery) catheter in situ during surgery.

The Swan-Ganz catheter: friend or foe?

Several studies have shown outcome benefit from flow directed haemodynamic manipulation in the high risk surgical patient using either invasive^{3,4} or non-invasive^{5,6} monitoring techniques. Only sporadic studies have demonstrated an advantage for the critically ill ICU patient.⁷ However, a recent retrospective study by Connors and colleagues⁸ suggested that patients receiving a Swan-Ganz catheter on day 1 of their ICU admission were 39% more likely to die compared with patients matched for disease and illness severity by complex statistical manipulations who did not receive the catheter. The accompanying editorial⁹ advocated an immediate moratorium on catheter use, a situation¹⁰ paralleling an earlier study by Gore *et al.*,¹¹ who found an increase in mortality in patients with acute myocardial infarction, the only perceived change in management over historical controls being the increased use of Swan-Ganz catheters.

The study by Connors *et al* has been heavily criticised; nevertheless, it served as the catalyst for a recent US consensus meeting,¹² which acknowledged the lack of conclusive data showing benefit or harm, yet reaffirmed its likely worth. A prospective, randomised trial

rather than an immediate ban was recommended, a view supported by the US Food and Drug Administration.

It is more likely that fault, if any, lies with how the catheter is used rather than from any intrinsic damage caused by the catheter itself. To contemplate a study comparing management using the Swan-Ganz catheter against bedside clinical acumen alone undermines Ludwig's maxim and is, in my opinion, badly misdirected. A number of studies in both intensive care^{7,13,14} and coronary care unit^{15,16} populations has shown the unreliability of clinical and radiological evaluation of haemodynamic status with experienced specialists faring no better than junior staff and medical students.¹³ A first priority in evaluating the Swan-Ganz catheter should be to ensure adequate training. A recent European questionnaire¹⁷ examining proper use and interpretation of data mirrored an earlier US study¹⁸ showing that competency was highly variable, with only 70% of questions being answered correctly. Second, how the catheter is used must be addressed. At the time of Connors *et al*'s study,⁸ many ICUs had adopted the supranormalised oxygen delivery philosophy advocated by Shoemaker whereby the circulation was driven with fluid loading followed by increasing doses of dobutamine to obtain predetermined raised values in cardiac index, oxygen delivery, and consumption.³ This approach proved highly successful in high risk non-cardiac surgical patients^{3,4} and was subsequently adopted by many ICUs. However, it took several years before—at best—no benefit¹⁹ and—at worst—harm²⁰ was demonstrated in such critically ill patients in prospective, randomised, controlled studies.

Non-invasive techniques

Several non-invasive techniques exist for flow monitoring but none has yet penetrated clinical practice to any great extent. The major issues are reliability and familiarity. Unfortunately, many commercial devices have been launched without proper validation and often with obvious design flaws. Furthermore, thermodilution, an imperfect gold standard,^{21,22} which is often used imperfectly,^{17,18} is often used as the comparator technique. These problems have served to undermine confidence in the various technologies, which upgraded equipment and newer models have yet to fully overcome.

The two best described techniques are Doppler ultrasound and thoracic bioimpedance. Doppler technology has enjoyed a renaissance since the advent of combined Doppler echocar-

UCL Medical School,
Department of
Medicine, Rayne
Institute Building,
University Street,
London WC1E 6JJ, UK
M Singer

Correspondence to:
Dr Singer.
email: m.singer@ucl.ac.uk

Accepted for publication
16 January 1998

Table 1 Formulae used for stroke volume calculation by thoracic bioimpedance

Kubicek 1966	$\rho \cdot \frac{L^2}{(Z_0)^2} \cdot (dZ/dt)_{\max} \cdot LVET$
Sramek 1983	$\delta \cdot \frac{L^3}{4.25} \cdot \frac{(dZ/dt)_{\max}}{Z_0} \cdot LVET$
Sramek-Bernstein 1986	$\delta \cdot \frac{0.17H^3}{4.25} \cdot \frac{(dZ/dt)_{\max}}{Z_0} \cdot LVET$
Adjusted Kubicek 1997	$\rho \cdot \frac{(0.17H)^2}{(Z_0)^2} \cdot (dZ/dt)_{\max} \cdot LVET$

(dZ/dt)_{max}, maximum of 1st derivative of impedance signal; ρ, electrical resistivity of blood; L, distance between two levels of electrodes; δ, correction factor depending on weight; LVET, left ventricular ejection time; H, height; Z₀, basic thoracic impedance.

diography, in particular, from the transoesophageal approach, which has provided new possibilities for both diagnosis and monitoring.²³⁻²⁵ Some authorities advocate its superiority over invasive techniques²⁶; however, expense, complexity, and the necessary expertise have restricted its widespread application in the UK. A simpler technique uses stand-alone Doppler ultrasound that interrogates the blood vessel—usually ascending or thoracic descending aorta—from suprasternal^{27, 28} or oesophageal^{29, 30} approaches, respectively. This enables monitoring of blood flow velocity from which a reasonable estimate of cardiac output can be made. The shape of the flow velocity waveform also readily permits assessment of left ventricular contractility and filling, and systemic vascular resistance.^{30, 31} A Starling-type curve can be constructed from the stroke volume response to 200 ml fluid challenges. To date, oesophageal Doppler ultrasound is the only non-invasive technology used successfully to direct intraoperative fluid loading, resulting in outcome benefit and significant reductions in hospital stay in prospective, randomised, controlled trials of cardiac⁵ and orthopaedic⁶ surgery. A relevant finding from these studies was the greater sensitivity of stroke volume over cardiac output, as compensatory tachycardia tended to maintain cardiac output in the face of mild to moderate hypovolaemia. Thus, overall, the control groups showed no change in output but had significant falls in stroke volume.

An editorial³² accompanying the hip fracture repair study⁶ spelled out the potential benefits of this non-invasive flow monitoring technique in high risk patients undergoing surgery, but emphasised the need for multicentre confirmation before its widespread adoption. It is worth reiterating that outcome was improved by acting on the information provided to achieve the set goal of optimal filling. Which haemodynamic goals are applicable to different patient populations (high risk surgery, severe heart failure, sepsis), and whether non-invasive techniques are equal, or even superior, to invasive monitoring techniques requires extensive study, but encouragement can be drawn from these initial investigations.

Thoracic bioimpedance has had a more chequered course. In 1966 Kubicek described the thorax as a cylinder evenly perfused with blood of specific resistivity. In 1983 Sramek demonstrated that the thorax behaves electrically more

like a truncated cone. Pulsatile thoracic aortic blood flow causes negative impedance changes with a maximum rate of change during systole between pairs of electrodes placed on the neck and upper abdomen. Various new correction factors and equations have been advanced (table 1) and incorporated into commercial systems using pairs of electrodes placed around neck, thorax, and upper abdomen. Unfortunately, validation studies have produced highly inconsistent results. Generally, the technique appears to be reasonably reliable in healthy volunteers but performs unpredictably in the critically ill.³³⁻³⁷ Thus, the paper by Spiering *et al* in this issue³⁸ is rather surprising in view of the major discrepancy between bioimpedance and dye dilution in normal subjects. Despite the authors' assurances, I wonder if an unrecognised methodological problem affected the study outcome. If bioimpedance is to develop as a clinical tool it must address these reliability issues, alert the operator to erroneous readings, and regain user confidence.

Other techniques are also available for either intermittent or continuous monitoring of flow. Echocardiographic measurement of ventricular volumes at end systole and end diastole enables stroke volume to be measured with reasonable accuracy²³⁻²⁵; however, at least six different methods have been described and user expertise is a significant factor. Recently developed technology allows three dimensional reconstruction of images of the left ventricle, although ventricular volumes are still generally calculated from cross sectional and M mode images, accepting assumptions about left ventricular shape.

Analysis of the contour of the aortic pulse wave allows monitoring of cardiac output, as the rate blood flows from arteries to veins is proportional to the rate of fall of arterial pressure. This can be performed non-invasively from a finger probe³⁹ or from an indwelling pressure transduced arterial cannula.⁴⁰⁻⁴² There is not an extensive literature assessing its reliability in different conditions; furthermore, it cannot be used for measurement of cardiac output unless first calibrated against another technique.

Thermal dilution techniques can be performed without the need for pulmonary artery catheterisation,⁴³ although validation data are scanty. A commercially available device using this technology (COLD; Pulsion, Munich, Germany) also claims to measure global end diastolic volume (the sum of the end diastolic volumes of both left and right atria and ventricles), intrathoracic blood volume (a possible indicator of cardiac preload), and extravascular lung water.^{43, 44}

The Fick principle states that oxygen consumption (Vo₂) equals cardiac output multiplied by the arteriovenous oxygen concentration difference. For cardiac output measurement the arterial oxygen concentration is measured from a peripheral arterial blood sample, the venous oxygen concentration from pulmonary arterial blood, and Vo₂ is derived from minute ventilation and inspired and expired gas analysis.⁴⁵⁻⁴⁸ In a variation of this method, CO₂ production can be used instead of oxygen consumption although

large discrepancies have been found in comparative studies in the critically ill.⁴⁸ In theory, the Fick technique is the gold standard for cardiac output measurement but it is invasive and methodological error is not uncommon—for example, when high inspired oxygen concentrations are being administered. Using the indirect Fick approach, the carbon dioxide rebreathing technique is a popular technique among sports physiologists as it is totally non-invasive and more reliable at exercise than at rest.^{47 49 50} The rebreathing manoeuvre is used to estimate mixed venous P_{CO₂} (PV_{CO₂}), which, combined with end tidal P_{CO₂} and CO₂ production, gives a non-invasive Fick estimate of the cardiac output. Reproducibility is not as high as other techniques^{48 49} and it has yet to be applied at the bedside of the sick patient.

Finally, the dye dilution technique may enjoy renewed interest as a bedside cardiac output monitoring technique through online means of measuring plasma concentrations of indocyanine green, the standard indicator in use today.^{44 45 51} Alternatively, a new approach using lithium chloride as the indicator^{52 53} with plasma concentrations being measured by a lithium selective electrode in a flow through cell connected by a three way tap to a standard arterial cannula, may also merit consideration.

Conclusion

There is sufficient evidence to show that flow monitoring leading to directed haemodynamic management is beneficial, at least in certain patient subsets. Advantage is generally gained by those at risk of, rather than having, established organ failure, such as the high risk surgical patient. Few studies have demonstrated outcome benefit in critically ill patients in whom metabolic, inflammatory, and cellular processes are often too far advanced for benefit to be gained from haemodynamic manipulations that prevent or reverse tissue hypoxia, a potent stimulus of various inflammatory pathways. Current use of flow monitoring generally precludes pre-emptive circulatory optimisation to prevent, or at least, minimise tissue hypoxia. This is equally applicable to the trauma patient or the patient in acute heart failure, where hypovolaemia often passes unrecognised and untreated until hypotension and organ failure have supervened. Invasive measurement of cardiac output is coming under increasing scrutiny and the place of non-invasive technology merits re-appraisal in the light of newer and more reliable equipment and techniques. This should provide impetus for further investigation, particularly in patients in the early stages of illness.

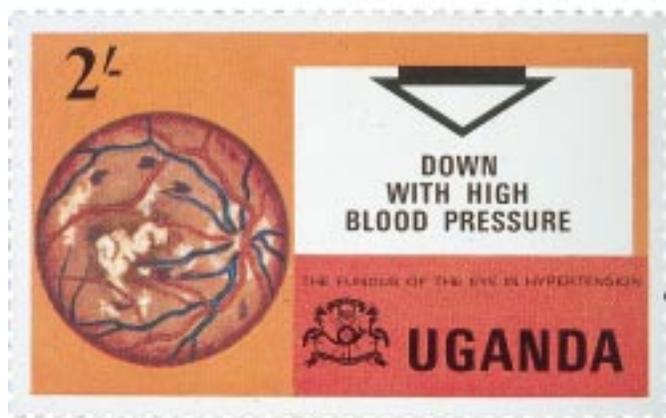
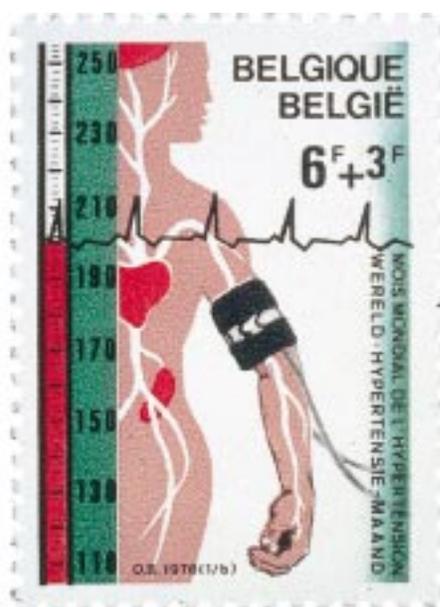
- 1 Singer M, Bennett ED. Invasive hemodynamic monitoring in the United Kingdom. Enough or too little? *Chest* 1989;95:623-6.
- 2 Report of the national confidential enquiry into perioperative deaths (NCEPOD) 1993/1994. London: Confidential Enquiry into Perioperative Deaths, 1996.
- 3 Shoemaker WC, Appel PL, Kram HB, et al. Prospective trial of supranormal values of survivors as therapeutic goals in high-risk surgical patients. *Chest* 1988;94:1176-86.
- 4 Boyd O, Grounds RM, Bennett ED. A randomised clinical trial of the effect of deliberate perioperative increase of oxygen delivery on mortality in high-risk surgical patients. *JAMA* 1993;270:2699-707.
- 5 Mythen MG, Webb AR. Perioperative plasma volume expansion reduces the incidence of gut mucosal hypoperfusion in cardiac surgery. *Arch Surg* 1995;130:423-9.

- 6 Sinclair S, James S, Singer M. Intraoperative intravascular volume optimisation and length of hospital stay after repair of proximal femoral fracture: randomised, controlled trial. *BMJ* 1997;315:909-12.
- 7 Mimoz O, Rauss A, Rezik N, et al. Pulmonary artery catheterization in critically ill patients: a prospective analysis of outcome changes associated with catheter-prompted changes in therapy. *Crit Care Med* 1994;22:573-9.
- 8 Connors AF Jr, Speroff T, Dawson NV, et al. The effectiveness of right heart catheterization in the initial care of critically ill patients. SUPPORT Investigators. *JAMA* 1996;276:889-97.
- 9 Dalen JE, Bone RC. Is it time to pull the pulmonary artery catheter? [editorial] *JAMA* 1996;276:916-18.
- 10 Robin ED. Death by pulmonary artery flow-directed catheter. Time for a moratorium? [editorial] *Chest* 1987;92:727-31.
- 11 Gore JM, Goldberg RJ, Spodick DH, et al. A community-wide assessment of the use of pulmonary artery catheters in patients with acute myocardial infarction. *Chest* 1987;92:721-7.
- 12 Pulmonary artery catheter consensus conference: consensus statement. *Crit Care Med* 1997;25:910-25.
- 13 Connors AF Jr, McCaffree DR, Gray BA. Evaluation of right heart catheterisation in the critically ill patient without acute myocardial infarction. *N Engl J Med* 1983;308:263-7.
- 14 Eisenberg PR, Jaffe AS, Schuster DP. Clinical evaluation compared to pulmonary artery catheterisation in the haemodynamic assessment of critically-ill patients. *Crit Care Med* 1984;12:549-53.
- 15 Bayliss J, Norell M, Ryan A, et al. Bedside haemodynamic monitoring: experience in a general hospital. *BMJ* 1983;287:187-90.
- 16 Timmis AD, Fowler MB, Burwood RJ, et al. Pulmonary oedema without critical increase in left atrial pressure in acute myocardial infarction. *BMJ* 1981;283:636-8.
- 17 Gnaegi A, Feihl F, Perret C. Intensive care physicians' insufficient knowledge of right-heart catheterization at the bedside: time to act? *Crit Care Med* 1997;25:213-20.
- 18 Iberti TJ, Fischer EP, Leibowitz-AB, et al. A multicenter study of physicians' knowledge of the pulmonary artery catheter. Pulmonary Artery Catheter Study Group. *JAMA* 1990;264:2928-32.
- 19 Gattinoni L, Brazzi L, Pelosi P, et al. A trial of goal-oriented hemodynamic therapy in critically ill patients. SvO₂ Collaborative Group. *N Engl J Med* 1995;333:1025-32.
- 20 Hayes MA, Timmins AC, Yau EH, et al. Elevation of systemic oxygen delivery in the treatment of critically ill patients. *N Engl J Med* 1993;330:1717-22.
- 21 Stetz CW, Miller RG, Kelly GE, et al. Reliability of the thermolimitation method in the determination of cardiac output in clinical practice. *Am Rev Respir Dis* 1982;126:1001-4.
- 22 Stevens JH, Raffin TA, Mihm FG, et al. Thermolimitation cardiac output measurement. Effects of the respiratory cycle on its reproducibility. *JAMA* 1985;253:2240-2.
- 23 Flachskampf F. Recent progress in quantitative echocardiography. *Curr Opin Cardiol* 1995;10:634-9.
- 24 Pai RG, Shah PM. Echocardiographic and other noninvasive measurements of cardiac hemodynamics and ventricular function. *Curr Probl Cardiol* 1995;20:681-770.
- 25 Troianos CA, Porembka DT. Assessment of left ventricular function and hemodynamics with transesophageal echocardiography. *Crit Care Clin* 1996;12:253-72.
- 26 Jardin F. PEEP, tricuspid regurgitation, and cardiac output. *Intens Care Med* 1997;23:806-7.
- 27 Huntsman LL, Stewart DK, Barnes SR, et al. Noninvasive Doppler determination of cardiac output in man. *Circulation* 1983;67:593-602.
- 28 Chandraratna PA, Nanna M, McKay C, et al. Determination of cardiac output by transcutaneous continuous-wave ultrasonic Doppler computer. *Am J Cardiol* 1984;53:234-7.
- 29 Singer M, Clarke J, Bennett ED. Continuous hemodynamic monitoring by esophageal Doppler. *Crit Care Med* 1989;17:447-52.
- 30 Singer M, Bennett ED. Non-invasive optimization of left ventricular filling by esophageal Doppler. *Crit Care Med* 1991;19:1132-7.
- 31 Singer M, Allen MJ, Webb AR, et al. Effects of alterations in left ventricular filling, contractility and systemic vascular resistance on the ascending aortic blood velocity waveform of normal subjects. *Crit Care Med* 1991;19:1138-45.
- 32 Arrowsmith JE, Gan TJ. The oesophageal Doppler monitor [editorial]. *BMJ* 1997;315:893-4.
- 33 Fuller HD. The validity of cardiac output measurement by thoracic impedance: a meta-analysis. *Clin Invest Med* 1992;15:103-12.
- 34 de May C, Matthews J, Butzer R, et al. Agreement and reproducibility of the estimates of cardiovascular function by impedance cardiography and M-mode echocardiography in healthy subjects. *Br J Clin Pharmacol* 1992, 34:88-92.
- 35 Appel P, Kram HB, Mackabee J, et al. Comparison of measurements of cardiac output by bioimpedance and thermolimitation in severely ill surgical patients. *Crit Care Med* 1986;14:933-5.
- 36 Preiser JC, Daper A, Parquier JN, et al. Transthoracic electrical bioimpedance versus thermolimitation technique for cardiac output measurement during mechanical ventilation. *Intens Care Med* 1989;15:221-3.
- 37 Young JD, McQuillan P. Comparison of thoracic electrical bioimpedance and thermolimitation for the measurement of cardiac index in patients with severe sepsis. *Br J Anaesth* 1993;70:58-62.

- 38 Spiering W, van Es PN, de Leeuw PW. Comparison of impedance cardiography and dye dilution for measuring cardiac output. *Heart* 1998;79:437-41.
- 39 Gratz I, Kraidin J, Jacobi AG, *et al.* Continuous noninvasive cardiac output as estimated from the pulse contour curve. *J Clin Monit* 1992;8:20-7.
- 40 English JB, Hodges MR, Sentker C, *et al.* Comparison of aortic pulse-wave contour analysis and thermodilution methods of measuring cardiac output during anaesthesia in the dog. *Anesthesiology* 1980;52:56-61.
- 41 Tannenbaum GA, Mathews, Weissman C. Pulse contour cardiac output in surgical intensive care unit patients. *J Clin Anesth* 1993;5:471-8.
- 42 Irlbeck M, Forst H, Briegel J, *et al.* Continuous measurement of cardiac output with pulse contour analysis. *Anaesthetist* 1995;44:493-500.
- 43 Hoefl A, Schorn B, Weyland A, *et al.* Bedside assessment of intravascular volume status in patients undergoing coronary artery bypass surgery. *Anesthesiology* 1994;81:76-86.
- 44 Haller M, Zollner C, Briegel J, *et al.* Evaluation of a new continuous thermodilution cardiac output monitor in critically ill patients: a prospective criterion standard study. *Crit Care Med* 1995;23:860-6.
- 45 Neuhoef H, Wolf H. Method for continuously measured oxygen consumption and cardiac output for use in critically ill patients. *Crit Care Med* 1978;6:155-61.
- 46 Axler O, Tousignant C, Thompson CR, *et al.* Comparison of transesophageal echocardiographic, Fick, and thermodilution cardiac output in critically ill patients. *J Crit Care* 1996;11:109-16.
- 47 Espersen K, Jensen EW, Rosenborg D, *et al.* Comparison of cardiac output measurement techniques: thermodilution, Doppler, CO₂-rebreathing and the direct Fick method. *Acta Anaesthesiol Scand* 1995;39:245-51.
- 48 Sherman MS, Kosinski R, Paz HL, *et al.* Measuring cardiac output in critically ill patients: disagreement between thermodilution-, calculated-, expired gas-, and oxygen consumption-based methods. *Cardiology* 1997;88:19-25.
- 49 Russell AE, Smith SA, West MJ, *et al.* Automated non-invasive measurement of cardiac output by the carbon dioxide rebreathing method: comparisons with dye dilution and thermodilution. *Br Heart J* 1990;63:195-9.
- 50 Auchinloss JH, Gilbert R, Kuppinger M, *et al.* Mixed venous PCO₂ tension during exercise. *J Appl Physiol* 1980;48:933-8.
- 51 Iijima T, Aoyagi T, Iwao Y, *et al.* Cardiac output and circulating blood volume analysis by pulse dye-densitometry. *J Clin Monit* 1997;13:81-9.
- 52 Linton RAF, Band DM, Haire KM. A new method of measuring cardiac output in man using lithium dilution. *Br J Anaesth* 1993;71:262-6.
- 53 Linton R, Band D, O'Brien T, *et al.* Lithium dilution cardiac output measurement: a comparison with thermodilution. *Crit Care Med* 1997;25:1796-800.

STAMPS IN CARDIOLOGY

Hypertension



The theme for the 1978 World Health Day was "Down with high blood pressure". A number of countries issued stamps to promote this campaign. Four stamps and a miniature sheet (containing the complete set) were released by Uganda. Illustrated is the 2 shilling stamp which incorporates the campaign slogan and hypertensive retinal changes. (The other three stamps depicted a sphygmomanometer and a daily blood pressure chart, the heart in hypertension, and the kidneys and renal circulation.) Belgium issued a set of three charity stamps in 1978 for philanthropic works; the middle 6 franc value (carrying a 3 franc surcharge) contained the stamp for the World Health Day. The design incorporates the measurement of blood pressure, a stylised heart, brain, and kidney as well as the electrocardiogram. (The other two stamps in the set featured deserted children and the De Mick sanatorium (antituberculosis campaign issue).)

Hypertension and the measurement of blood pressure have appeared on a few stamps outside of the 1978 World Health Organisation theme. These include stamps from Czechoslovakia in 1952 for the National Health Service, the United Nations (Vienna headquarters) in 1988 for international volunteer day and in 1983 from the British Virgin Islands for nursing week.

M K DAVIES
A HOLLMAN