

cardiac CT that are summarised in Abstract 111 table 1. These incidental findings resulted in further investigations, documented in Abstract 111 table 2. The mean radiation dose ( $\pm$  SEM) for CAC scoring was  $0.61 \pm 0.03$  mSv. The mean radiation dose ( $\pm$  SEM) for subsequent CTCA was  $2.66 \pm 0.32$  mSv in high pitch "flash" mode ( $n=27$ ),  $5.86 \pm 0.50$  mSv in prospective mode ( $n=64$ ) and  $17.15 \pm 1.68$  mSv in the retrospective mode ( $n=25$ ).

Abstract 111 Table 1 Incidental findings on cardiac CT

Area	Structure	Incidental Finding	n
Chest ( $n=27$ )	Lung parenchyma	Nodule $<1$ cm	5
		Emphysema	3
		Atelectasis	6
		Fibrosis	4
		Tumour recurrence	1
		Bronchiectasis	2
	Pleura	Effusion	2
		Calcification	2
	Lymph node	Adenopathy	2
	Liver	Cyst/Nodules	6
Abdomen ( $n=7$ )	Adrenal	Adenoma/metastasis	1
Diaphragm ( $n=5$ )		Hiatus Hernia	5
Vasculature ( $n=11$ )	Aorta	Dilatation	8
		Aneurysm	1
	Renal	Stenosis	1
	Coeliac	Stenosis	1

Abstract 111 Table 2 Further investigation of incidental findings on Cardiac CT

Investigation	n
Bone scintigraphy	1
Chest clinic referral	2
CT chest	4
DMSA	1
MR adrenals	1
MRA renal	1
Nephrology clinic referral	1
Pleural fluid aspiration	1
Ultrasound kidneys	1
Ultrasound liver	3

Abstract 111 Table 3 Investigations and referrals generated by incidental findings

Investigations or referrals	Number
Bone scintigraphy	1
Chest clinic referral	2
CT chest	4
DMSA	1
MR adrenals	1
MR cardiac	2
MRA renal	1
Nephrology clinic referral	1
Pleural fluid aspiration	1
Ultrasound kidneys	1
Ultrasound liver	3

**Conclusions** Despite 62 patients having a reassuring CAC score of zero, 8% of this group had evidence of non-calcified plaque, with one patient having obstructive CAD that required intervention. We conclude that

if strong clinical suspicion remains in patients with a CAC score of zero further coronary investigation may be warranted. Incidental findings are common, and can result in multiple further investigations for patients. Further research is needed to evaluate the added cost, clinical benefits and radiation exposure created by investigation of such incidental findings in the context of cardiac CT.

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## COMPUTED TOMOGRAPHIC CORONARY ANGIOGRAPHY TO SCREEN FOR ALLOGRAFT VASCULOPATHY AFTER HEART TRANSPLANTATION

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**Objective** To evaluate Computed Tomographic Coronary Angiography (CTA) as an alternative to Invasive Coronary Angiography (ICA) for the detection of Cardiac Allograft Vasculopathy (CAV).

**Background** CAV is an important cause of late mortality after heart transplantation (HT). Because patients are often asymptomatic, surveillance ICA is performed in our institution. CTA is effective for the diagnosis of coronary disease in non-transplant patients, but few studies have been done after HT.

**Methods** 117 HT patients, 1 to 24 years post transplant (mean=12 years SD $\pm$  6) underwent CT coronary artery calcification (CTCAC) followed by retrospective ECG gated coronary angiogram on a 64-slice scanner without the use of any  $\beta$ -blockers. Majority (89%) of patients had CTA within 24 h before ICA. The Agatston calcium score (CS) was calculated for all patients. The CTA images were systematically analysed for image quality and the presence of CAV (graded as significant if  $>50\%$  luminal stenosis) using a fifteen coronary segments model by an independent investigator blinded to the results of ICA.

**Results** CS ranged from 0 to 1681 (Mean=91.7 $\pm$ 275). Out of 77 patients with absent CS, 3 had significant CAV on ICA. Despite a mean resting heart rate of 82 bpm SD $\pm$ 13 and body mass index of 27 kg/m<sup>2</sup> SD $\pm$ 5, 81% of the CTA images were graded as excellent or satisfactory. For all the 1755 segments assessed by CTA irrespective of the image quality, CTA had sensitivity, specificity, positive and negative predictive values of 71%, 79%, 72% and 78% respectively for the detection of any CAV found by ICA. On a patient basis, CTA best performed in diagnosing CAV of more than 25% with sensitivity, specificity, positive and negative predictive values of 74%, 94%, 79%, and 92% respectively. None of the 61 patients with completely normal CTA had CAV on ICA. 83 (92%) out of 90 patients who responded to a patient survey preferred CTA to ICA as a screening test for CAV. Non-coronary cardiac and non-cardiac abnormalities were identified in 18% and 14% patients respectively.

**Conclusion** The study shows that CTA compares favourably with ICA in detecting CAV in heart transplant recipients, and may be a preferable screening technique because of its non-invasive nature, patient preference and yield of additional information. One has to exercise caution in just using CS in these patients as significant CAV can be missed out.

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## DUAL ENERGY CT IMPROVES DIFFERENTIATION OF CORONARY ATHEROSCLEROTIC PLAQUE COMPONENTS COMPARED TO CONVENTIONAL SINGLE ENERGY CT

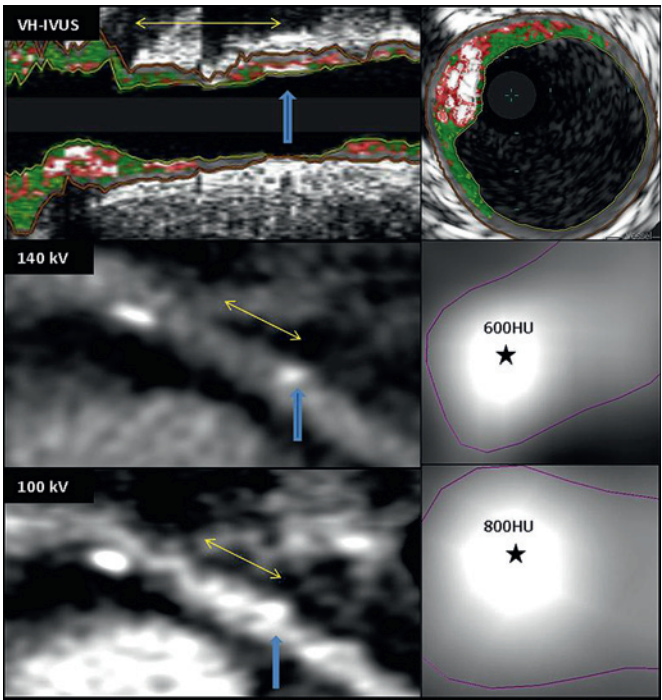
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**Introduction** Vulnerable plaques have a relatively high necrotic core area and low fibrous tissue content. Although CT can identify plaque components on the basis of their x-ray attenuation, there is

significant overlap between their attenuation ranges, most crucially between necrotic core and fibrous plaque. Recently introduced dual energy CT (DECT) permits acquisition of 2 different energy data sets simultaneously, with the change in attenuation of plaque components to different energies depending upon their material composition. We therefore examined whether DECT was better than single energy CT in determining plaque components defined by virtual histology IVUS.

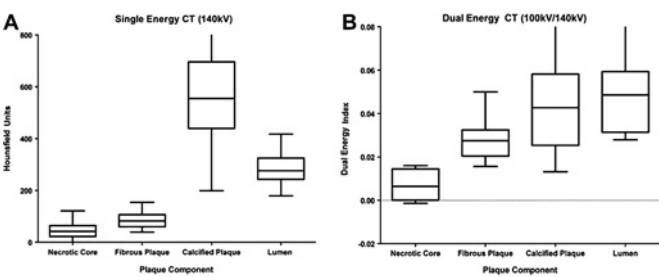
**Methods** 20 patients underwent DECT and 3-vessel VH-IVUS. CT data was obtained at peak voltages of 100 kV and 140 kV. 52 plaques were chosen with either homogenous fibrous plaque or confluent areas of calcified plaque or necrotic core as defined by VH-IVUS. VH-IVUS images were co-registered and orientated with the corresponding CT images using distance from coronary ostia and fiducial markers (Abstract 113 figure 1). Multiple regions of interest (ROI) were placed within the plaque components or in lumen on cross sectional CT images pre-classified by VH-IVUS (Abstract 113 figure 1). ROI densities were measured (in Hounsfield Units) and assigned to the plaque component. A dual energy index (DEI) was created for each component, defined as the ratio of the difference in attenuation at 2 different energies / sum of attenuation with 1000 added to each attenuation value to avoid negatives.



**Abstract 113 Figure 1** Demonstration of plaque co-registration between VH-IUS and 140kV/100kV CT data sets. Calcified plaque is identified 5mm from side branch adjacent to characteristic calcification (yellow line). Cross section taken through this plaque (blue arrow) and following orientation with VH-IVUS cross section HU region of interest sampling is performed in calcified plaque.

**Results** Attenuation values for 1088 ROIs were measured from 70 paired data sets at 100 kV and 140 kV creating 70 DEIs (12 necrotic core, 11 fibrous plaque, 29 calcified plaques and 18 lumen). Values obtained using a single energy data set showed good differentiation between calcified plaque and all others ( $p<0.05$ ), but considerable overlap between necrotic core and fibrous plaque ( $p=ns$ ) (Abstract 113 figure 2A) (Abstract 113 table 1). In DECT, lumen (iodinated contrast) showed the greatest change in attenuation and hence had the highest DEI. Necrotic core had the lowest DEI and could be distinguished from all other components ( $p<0.001$ ). Importantly, in contrast to the single energy data, DEI derived from both energy

data sets permitted resolution of necrotic core and fibrous plaque without overlap (Abstract 113 figure 2B).



**Abstract 113 Figure 2** (A) Defined CT attenuation spectra of plaque components using a single energy (140kV), calcified plaque is distinguishable from all others but necrotic core and fibrous plaque overlap. (B) The use of dual energy index from the attenuation data at 2 energies (100/140kV) allows significant separation of necrotic core and fibrous plaque ( $p<0.05$ ) (Tukeys multiple comparison test).

**Abstract 113 Table 1**

Plaque Component	100 kV mean HU (SD)	140 kV mean HU (SD)	Mean Difference (100–140 kV)	Dual Energy Index (mean)
Necrotic Core	57.26 (42.20)	42.69 (31.51)	14.57	0.0071
Fibrous Plaque	148.30 (49.47)	84.60 (30.34)	63.69	0.0283
Calcified Plaque	733.10 (226.7)	582.20 (194.9)	150.9	0.0450
Lumen	411.5 (82.27)	282.90 (55.93)	128.6	0.0483

**Conclusions** The additional attenuation data provided by DECT improves the differentiation of plaque components when compared to conventional single energy CT. In particular, DECT may allow better differentiation of necrotic core and fibrous plaque, a weakness of conventional cardiac CT, allowing for more accurate non-invasive identification of vulnerable plaques.

**114 RADIATION DOSES TRENDS FROM CARDIAC CT USING A CARDIAC SPECIFIC CONVERSION FACTOR: SYSTEM UNDERSTANDING & AN OPTIMISATION STRATEGY SIGNIFICANTLY REDUCES THE DOSE TO THE PATIENTS IN A CLINICAL SERVICE**

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**Background** CT coronary angiography CTCA now has an established role in the investigation of patients with chest pain. Under the IRMER regulations radiation doses to patients should be kept as low as reasonably practical (ALARP). Previous publications have used a chest conversion factor to calculate the effective dose (mSv) from CTCA. We have previously demonstrated that chest conversion factors significantly under-estimate the effective dose to the patient when applied to CTCA and have calculated a cardiac specific conversion factor of 0.028 mSv (mGy.cm)-1. Our department follows the ALARP ethos and has implemented new technologies together with physician training to reduce the radiation dose from CTCA. We aimed to investigate what impact the implementation of new technologies has had on the radiation dose of CTCA.

**Method** All patients who were coded as attending for a cardiac CT scan on the PACS and CRIS systems were included in the analysis. Scan indication included: rule out coronary artery disease, CABG assessment, pre-EP studies and problem solving. CT scanning